



Radiation Therapy Treatment Delivery Systems

Modern Technologies and Future Directions





Pedro Cardoso

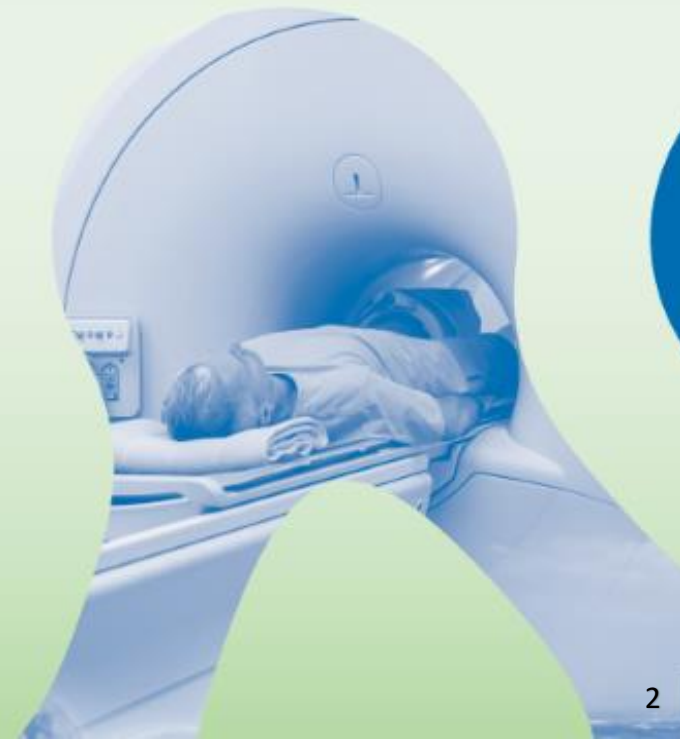
Medical Physicist @ Hospital Vila Nova Star





Overview

-  What is Radiation Therapy (RT) and how it's done
-  What's "mainstream" in modern RT delivery technology
-  What's trending
-  What might be coming

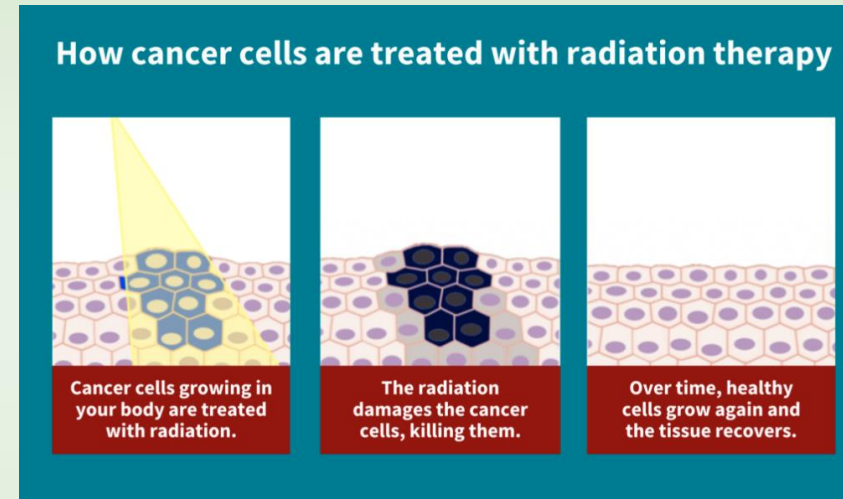


Radiation Therapy

- Use of ionizing radiation to treat diseases
- Mostly used to target and destroy cancer cells



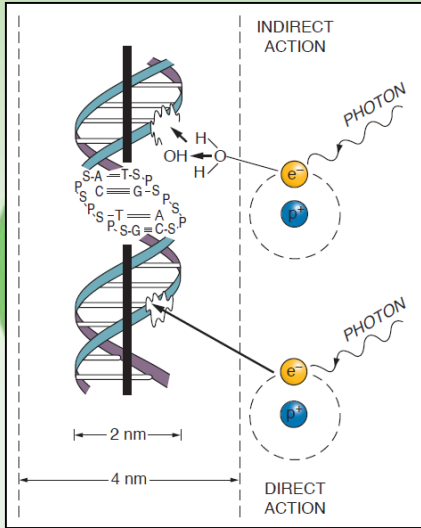
YouTube: UPMC



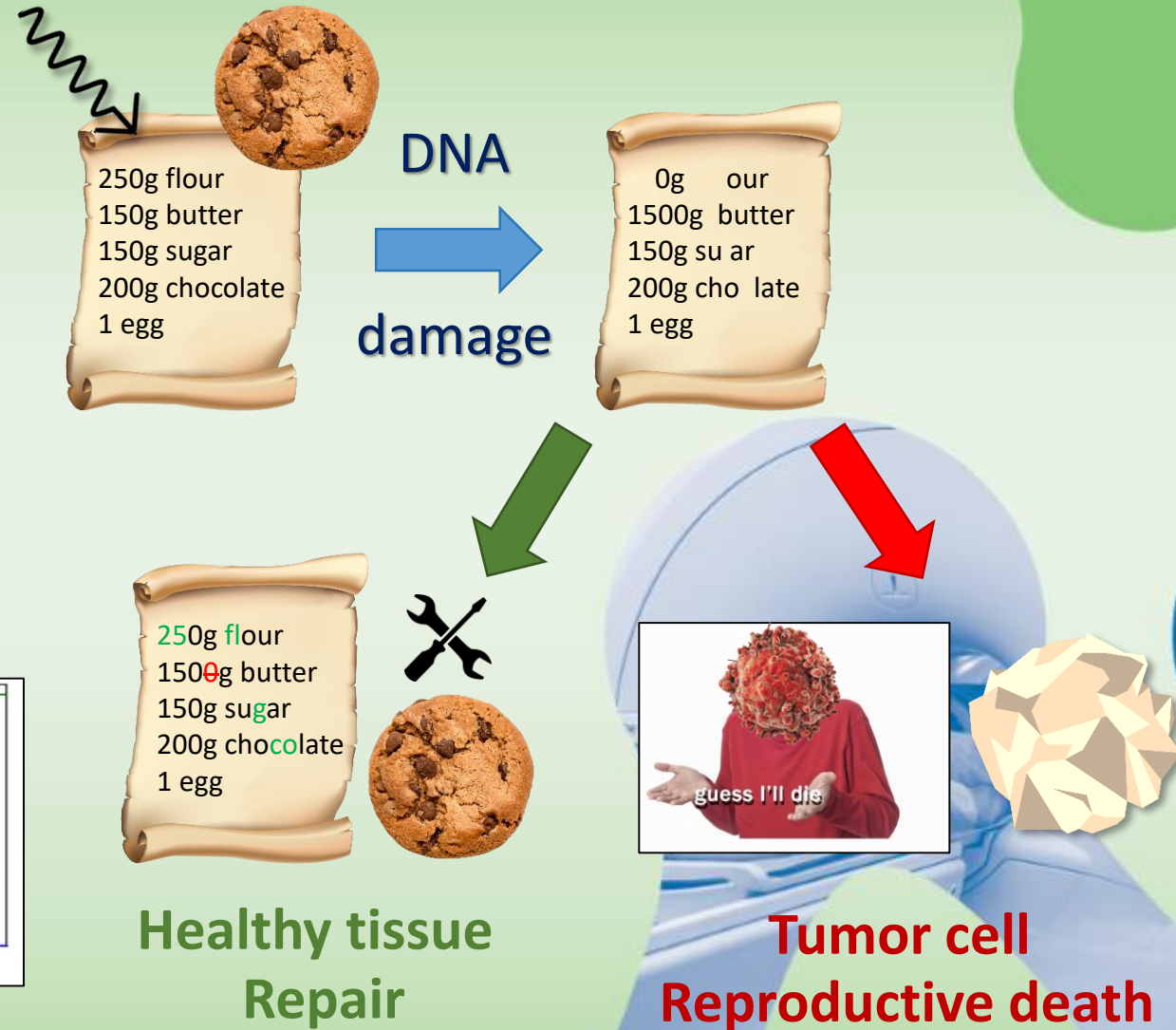
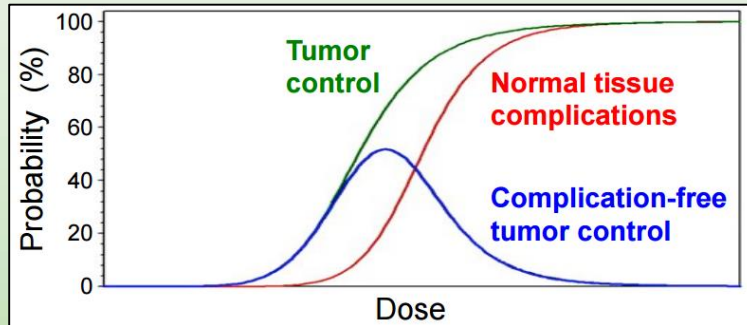
Stanford Medicine

- Radiation sources can be natural (radionuclides) or artificial (particle accelerators)
- In Brazil, the applications of radiation in therapy date from the 1920s

Radiation Therapy

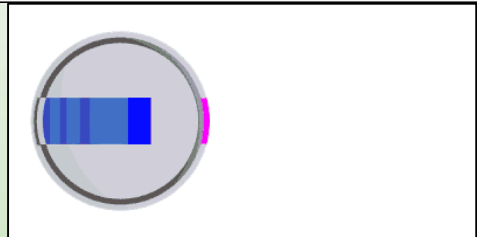
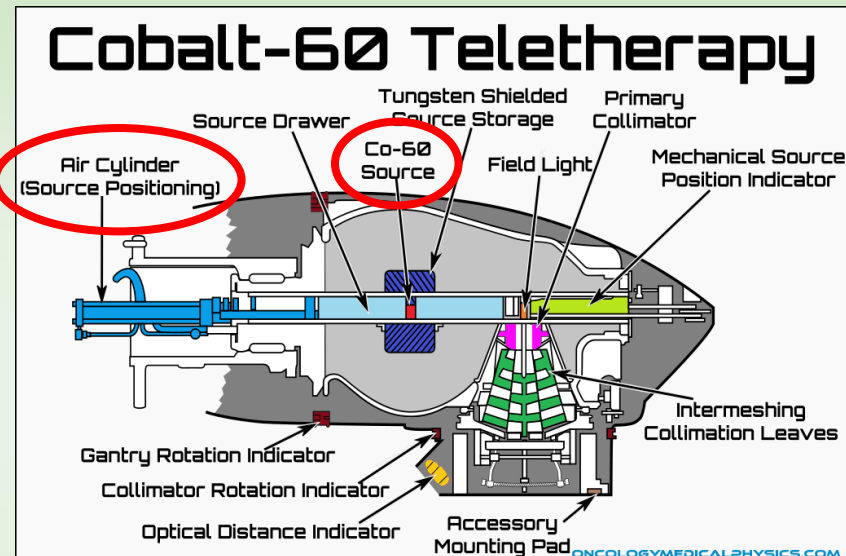


- Ionizing radiation can damage the DNA
- Healthy tissue can repair some of the damage
- With correct dose and fractionation, we can destroy more cancer cells than healthy tissue



Radionuclide units

- Gamma radiation (Cobalt-60 and Cesium-137)



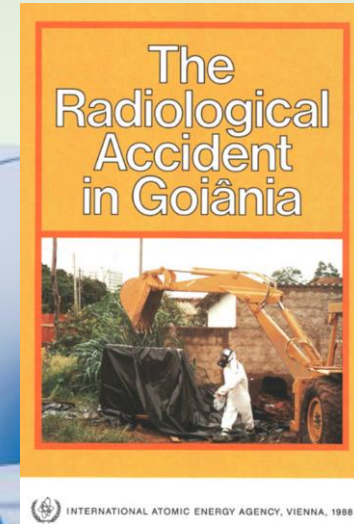
- Very uncommon in the developed world
 - In Brazil: 20 cobalt-60 units in 2019
- Still common in developing countries
 - Simplicity (source calibration and maintenance)

1987 Goiânia, Brazil

Deactivated Cs-137 stolen
Source capsule broken

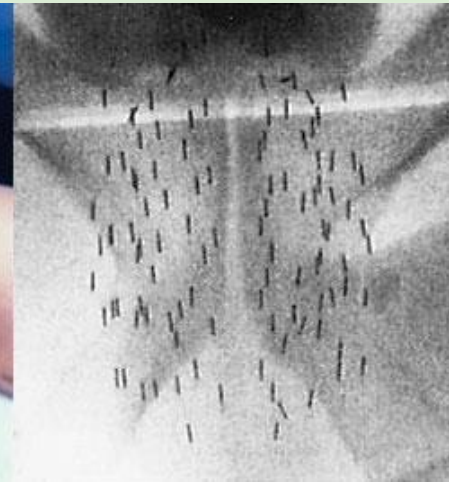
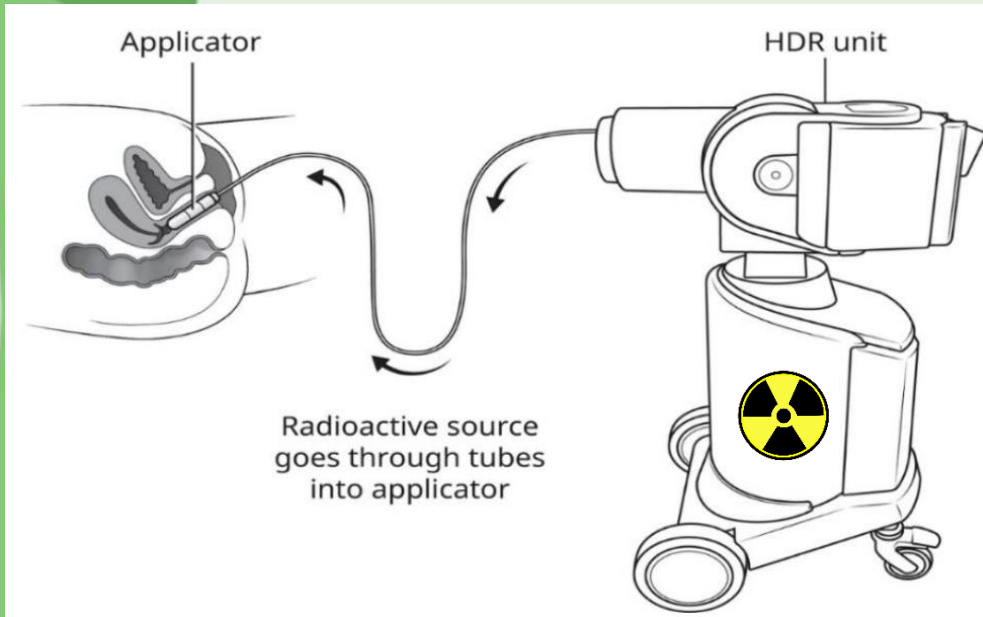


“Special mention must be made of **CNEN**, which coordinated the response to the accident within Goiás' State and at the national and international levels.”



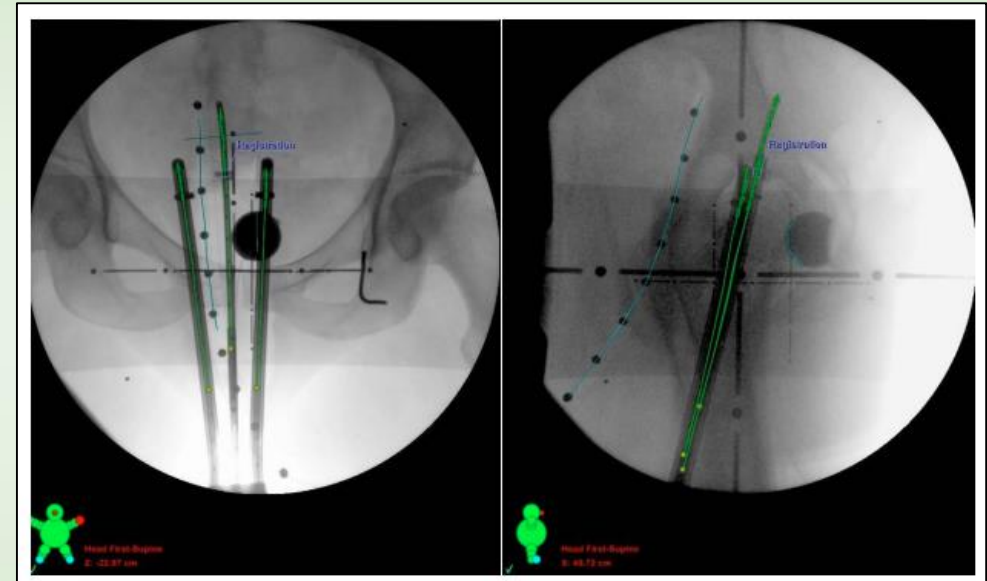
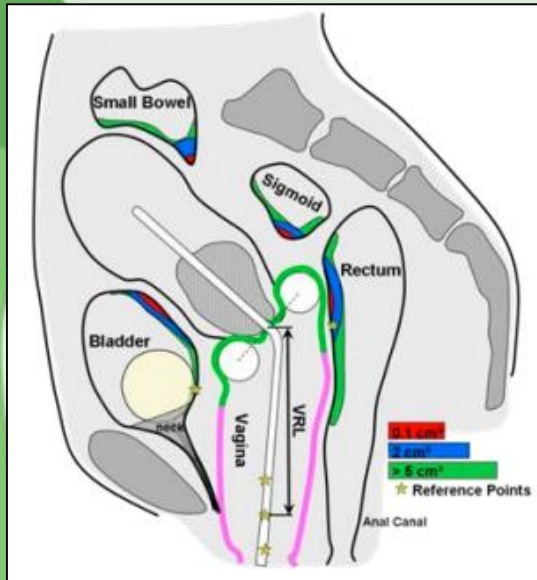
Brachytherapy (BT)

- Use of small radioactive sources in close proximity to the target
- Intracavitary, implants (seeds and wires) or contact



Brachytherapy (BT)

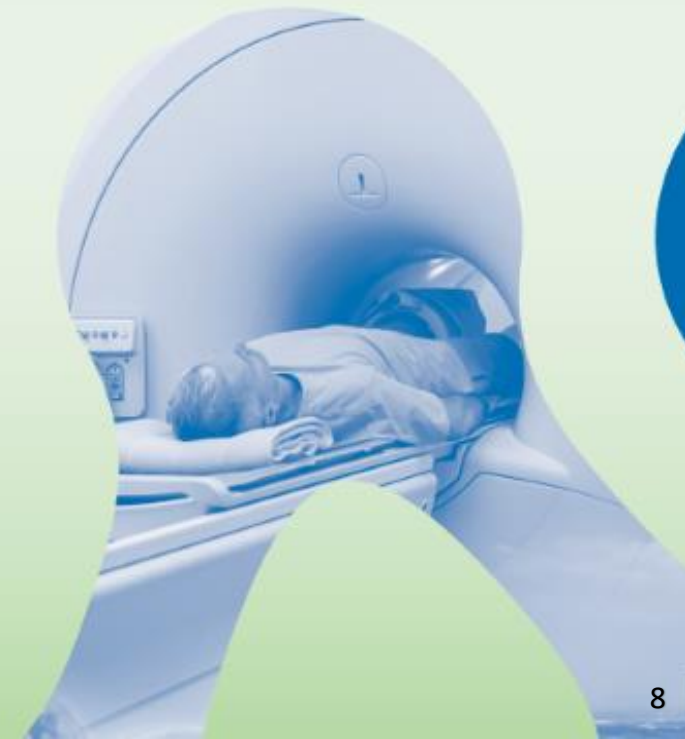
- In Brazil, >95% of BT procedures are gynecological (only site covered by the national public health insurance)



- Has been in decline worldwide
- Ex: in USA, GYN patients that received BT went from $\approx 85\%$ in 1990 to $\approx 60\%$ in 2010

Linear accelerators (LINACs)

- Most common source of radiation in RT (photons and electrons)
- Replaced most cobalt and cesium in the 1960s-1980s
- In Brazil, first Linac in 1971, 363 Linacs in 2018



LINAC: Beam production

- Injection Gun
 - Source of electrons
 - Thermionic effect of heated filament



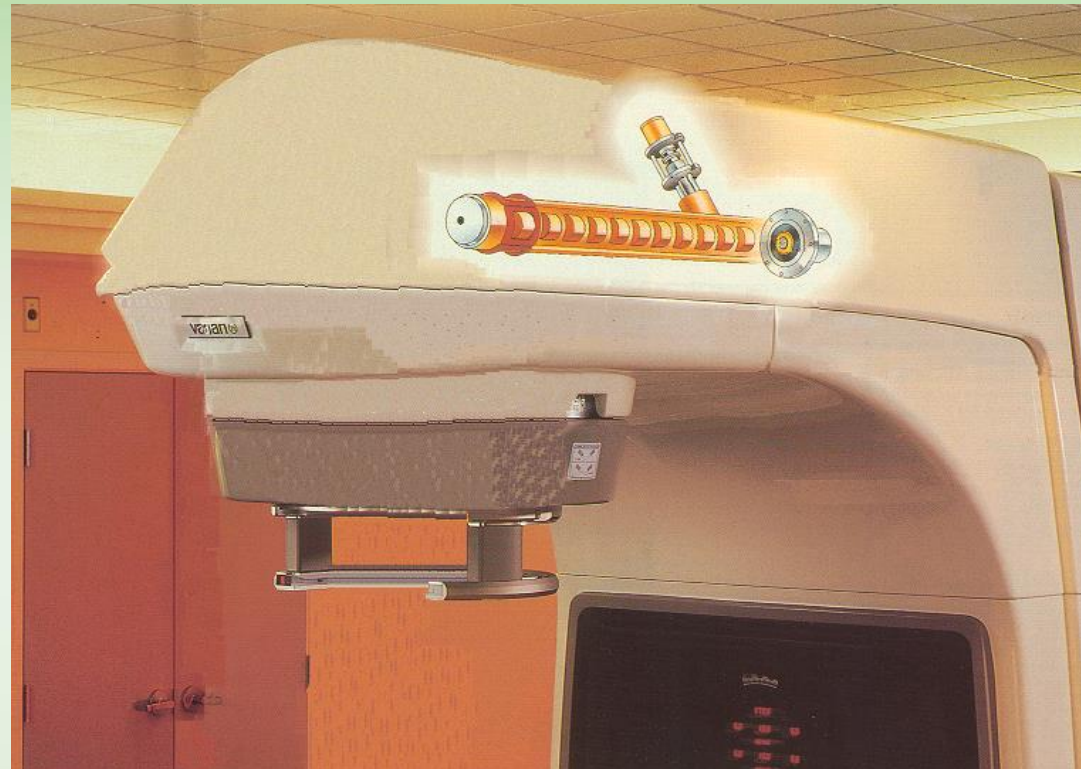
LINAC: Beam production

- Accelerator tube
 - Accelerates electrons with microwaves in resonating cavities
 - Most common energy used in RT is 6MV, but there are usually a few discrete options of higher energies



LINAC: Beam production

- Microwave source
- Magnetron (generator) and klystron (amplifier)



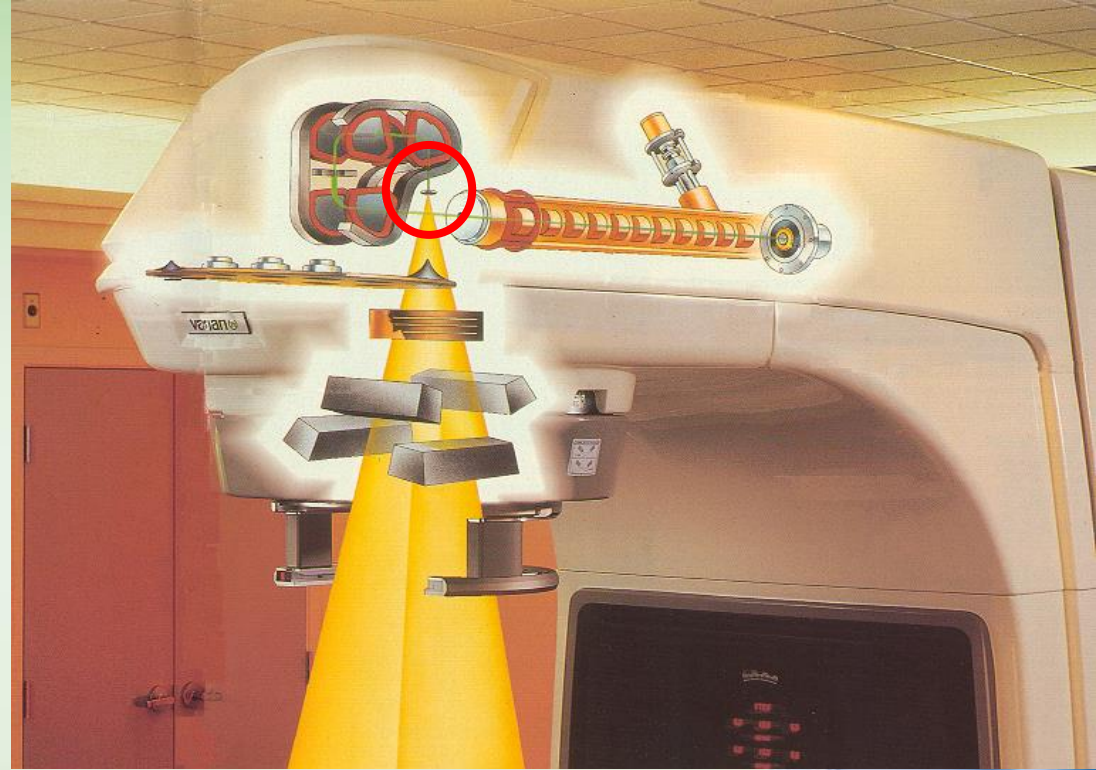
LINAC: Beam production

- Bending magnets
 - Redirects the electron beam towards the patient
 - Acts as energy filter



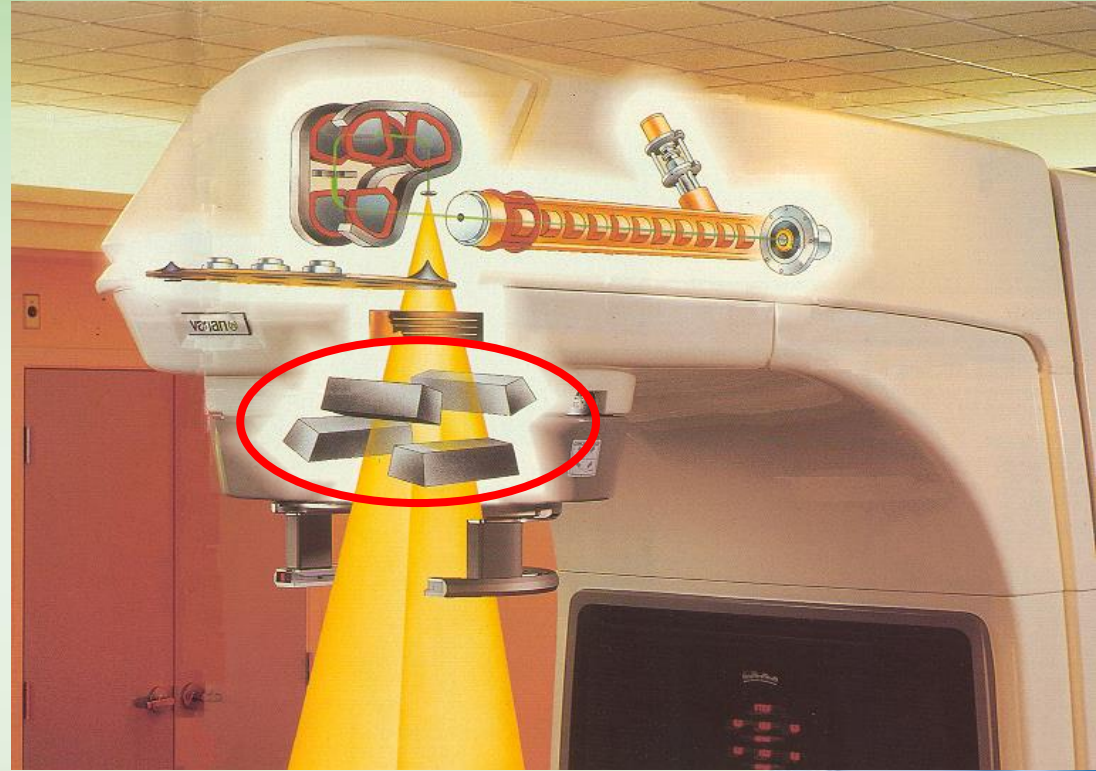
LINAC: Beam production

- Target
 - Tungsten disc
 - Produces X-Ray photons through deceleration of the incident electrons (bremsstrahlung)



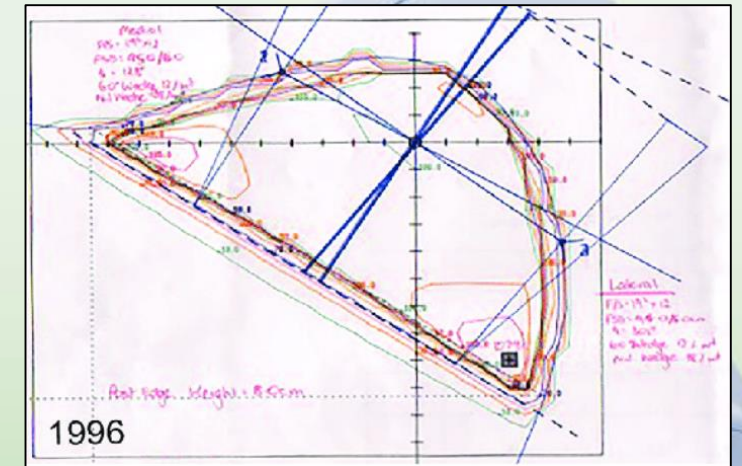
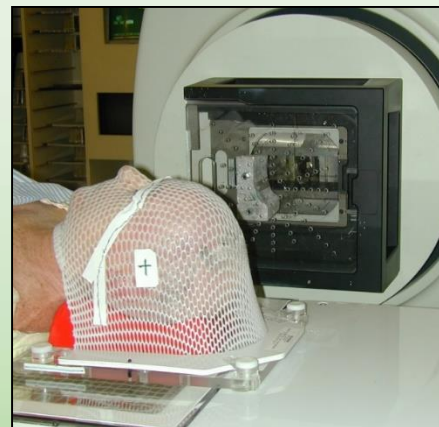
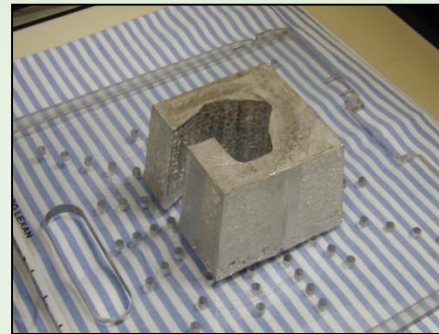
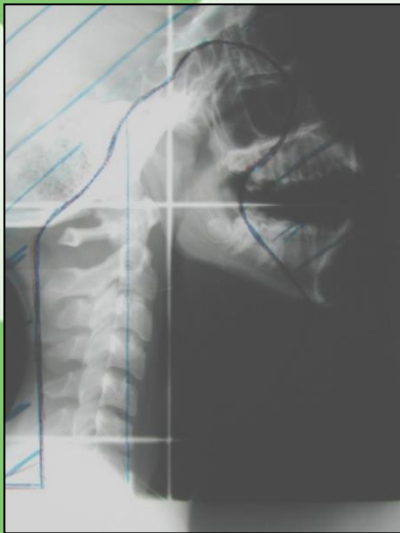
LINAC: Beam production

- Collimators
- Shape the beam into desired clinical shape



Early treatments: 2-Dimensional

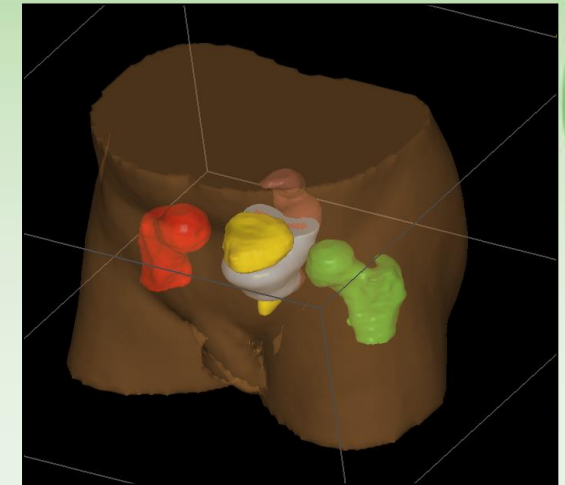
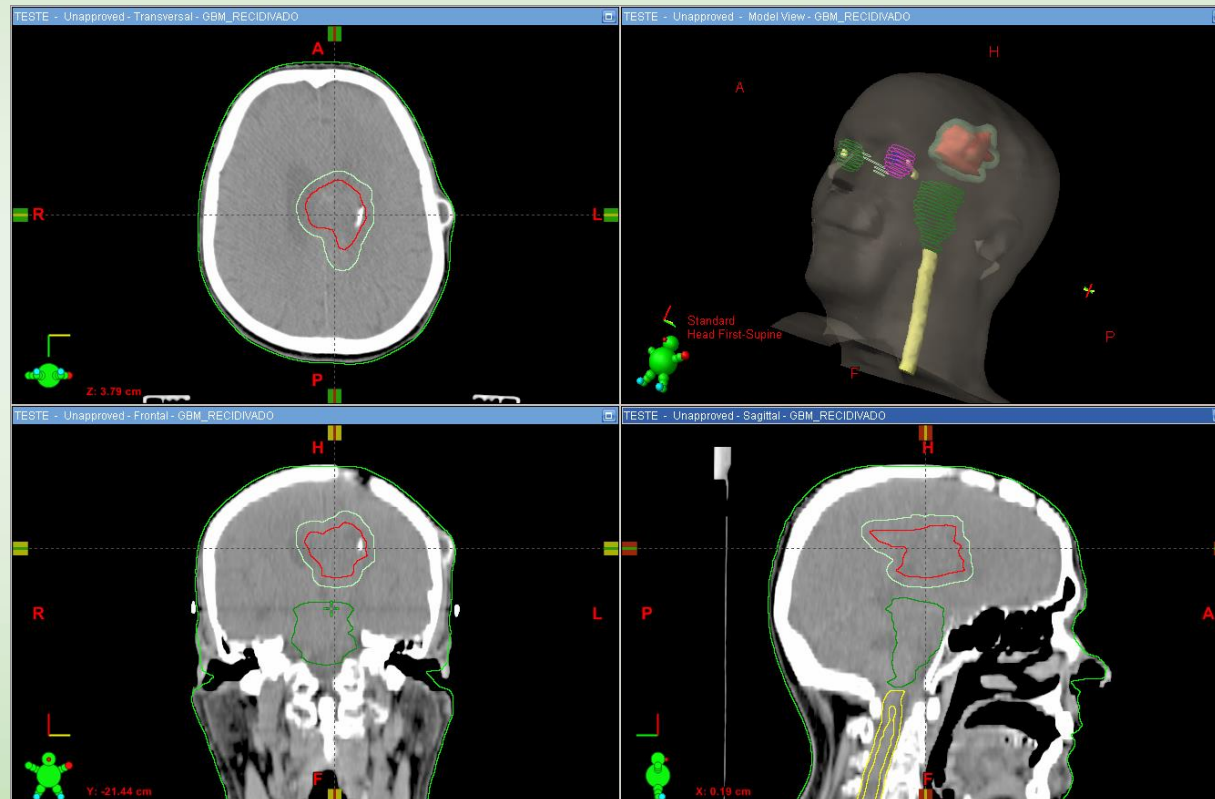
- Treatment region based on planar images, usually very overestimated
- Beam shaping done with metal blocks mounted on trays
- Simple beam configuration and manual dose calculation



3-Dimensional RT



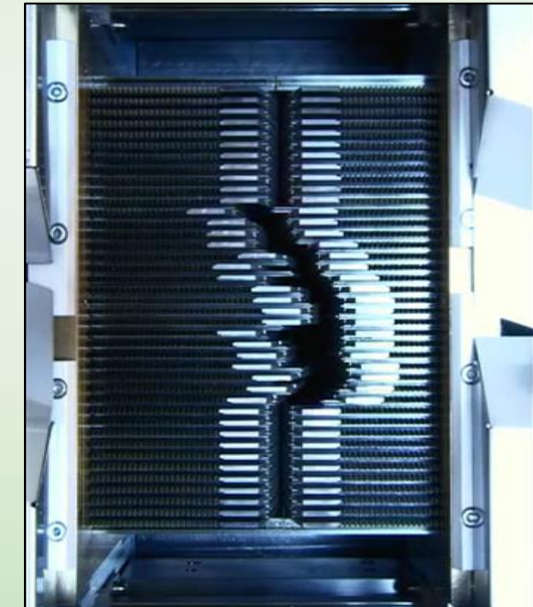
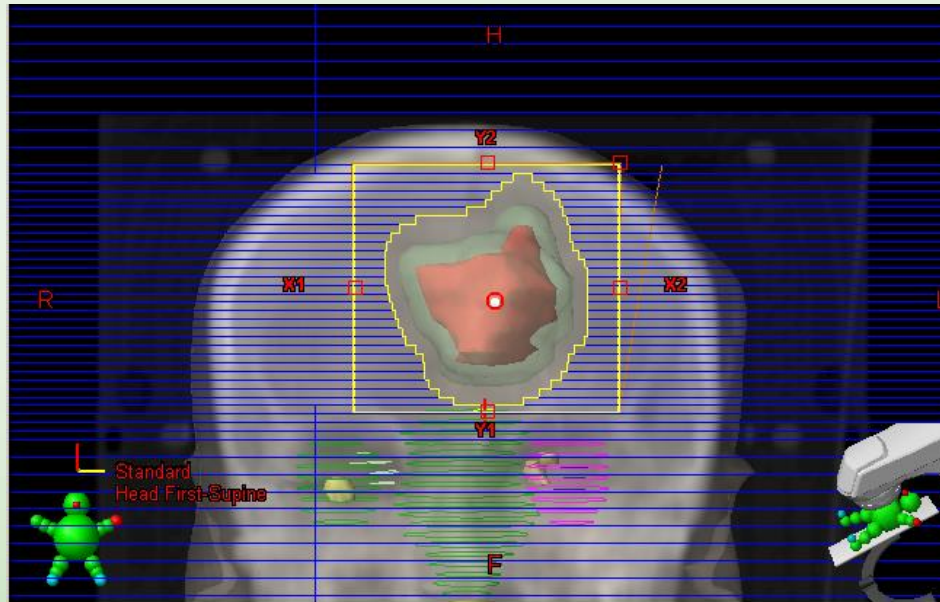
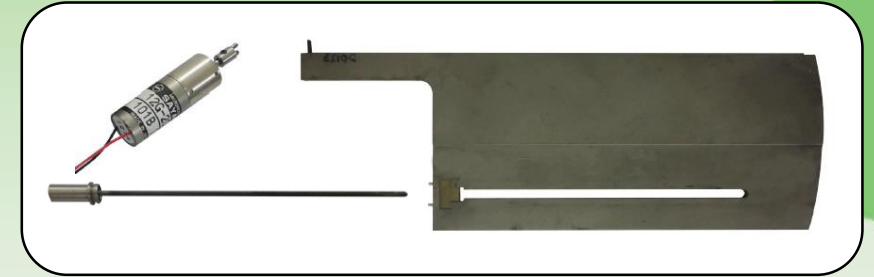
- Targets and organs-at-risk are defined in volumetric images (CT)



Multileaf collimators (MLC)

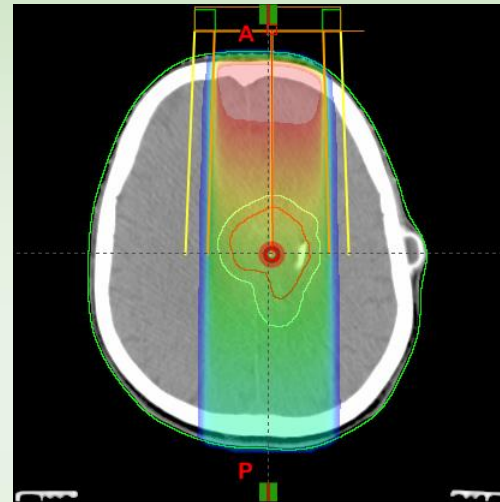
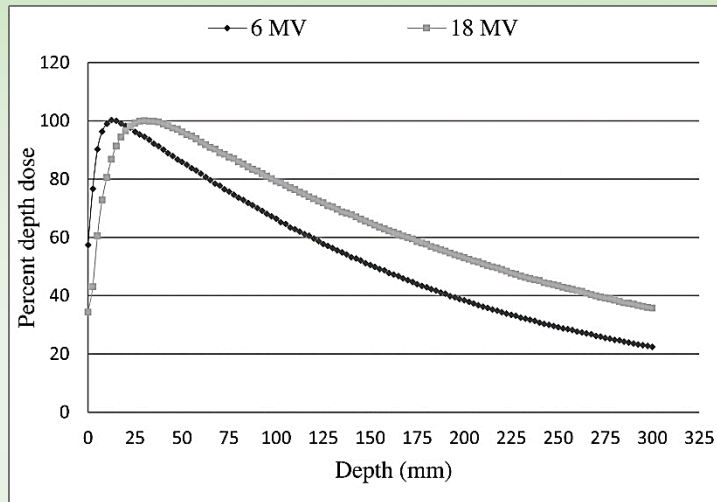


- 1980s-1990s (first in Brazil in 1995)
- Tungsten leaves with individual motors
- Capable of dynamic beam shaping



X-Ray Dose distribution

- X-ray dose deposition decreases with depth

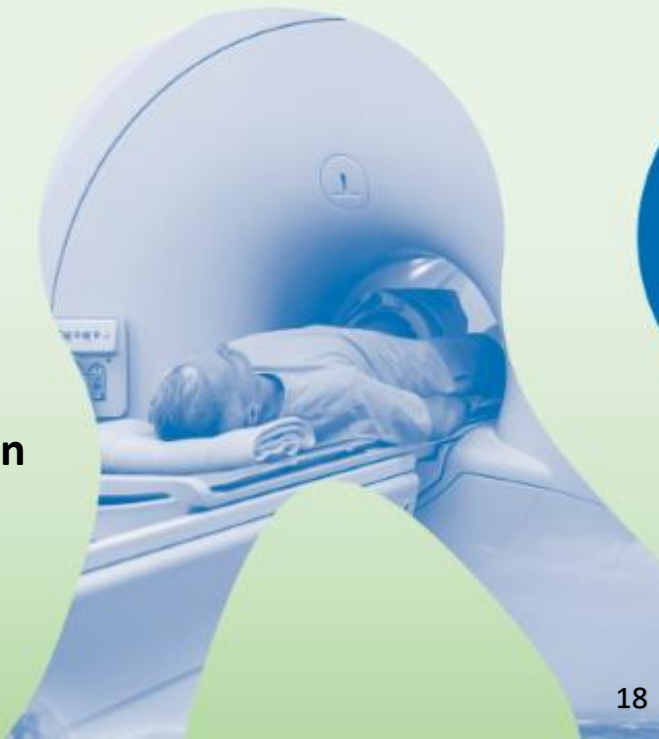


Single beam is often unacceptable

$$D(d) \propto \left(\frac{1}{d}\right)^2 \cdot e^{-d} \cdot k_s(d)$$

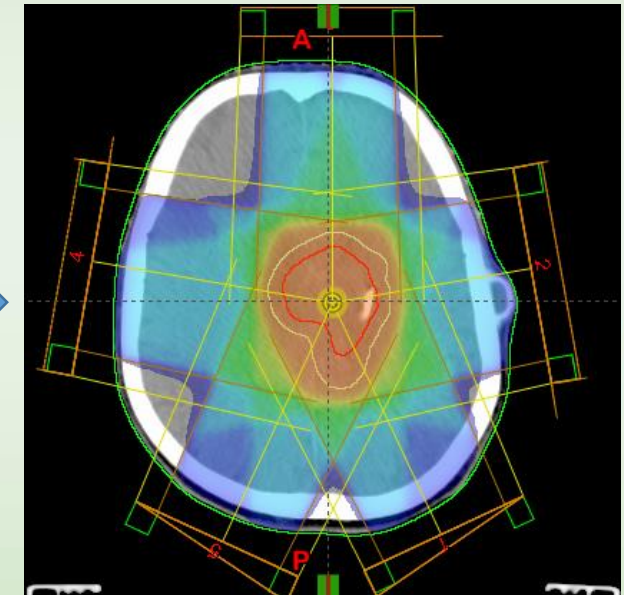
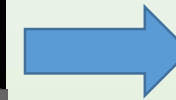
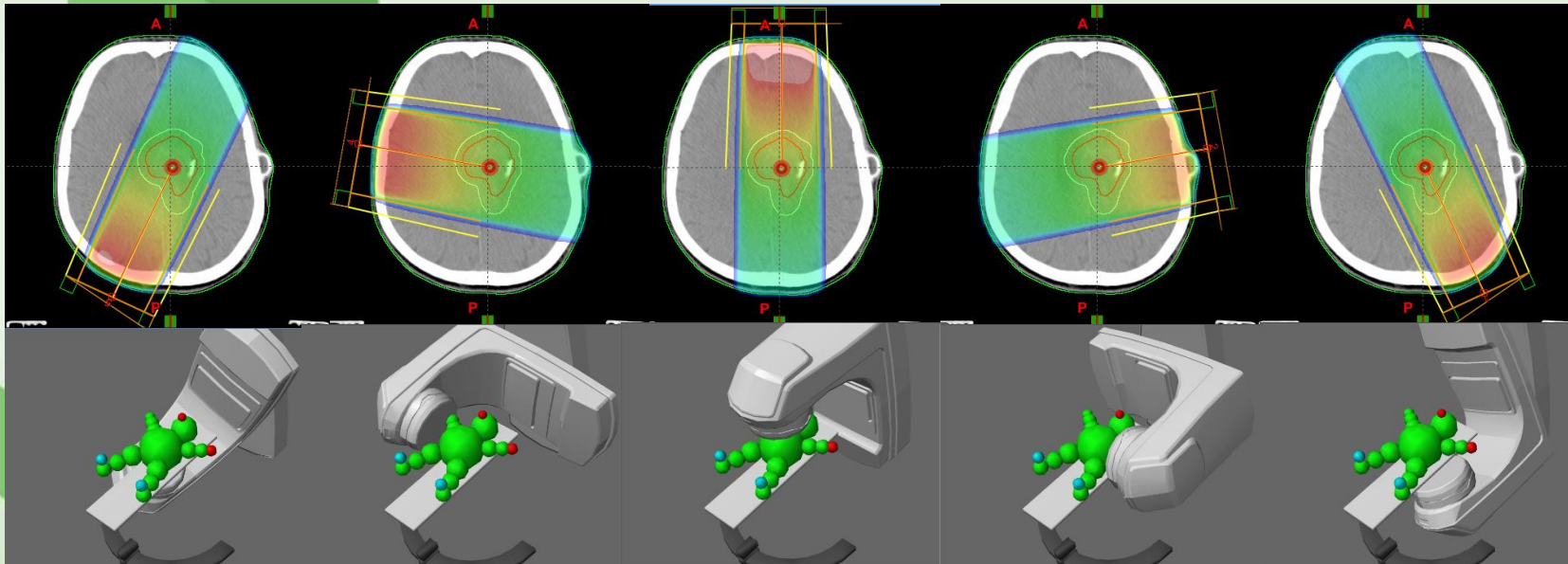
Annotations for the equation:

- inverse square distance (points to $\left(\frac{1}{d}\right)^2$)
- exponential attenuation (points to e^{-d})
- scatter (points to $k_s(d)$)



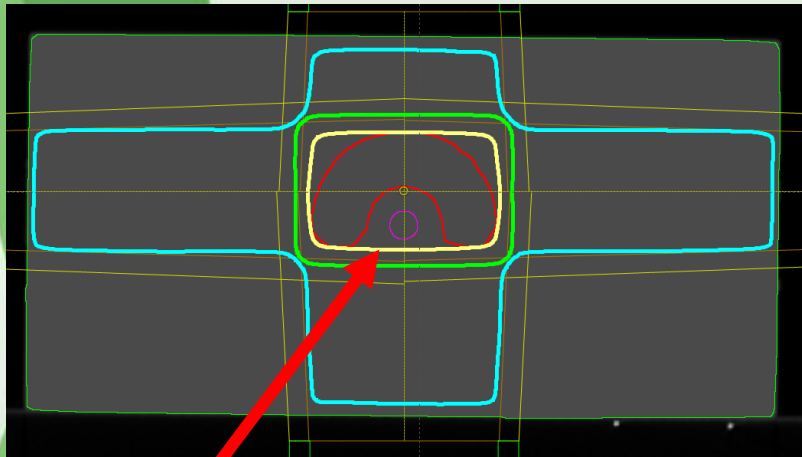
3D Conformal (3DCRT)

- Use of multiple beams to conform the dose to the target shape
- Treatment planning system (TPS) software used for dose calculation



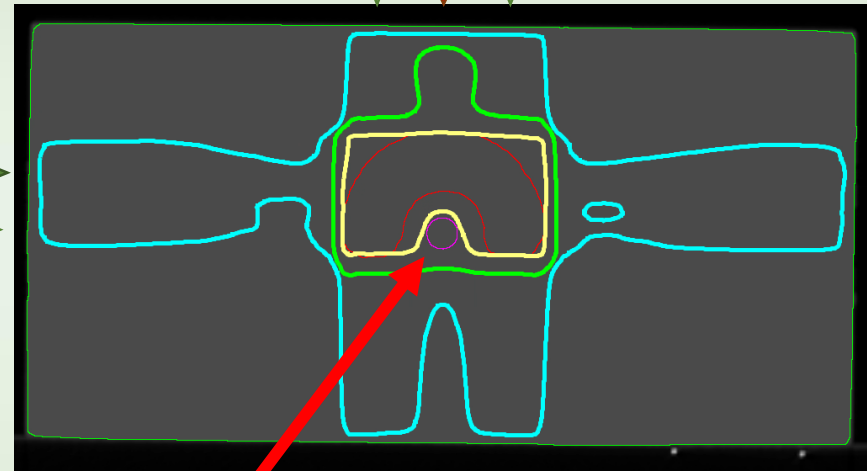
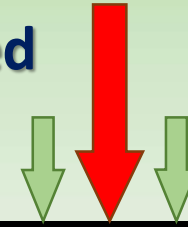
Beam modulation

Homogeneous beams



Healthy normal tissue inside a concave target receiving high dose of radiation

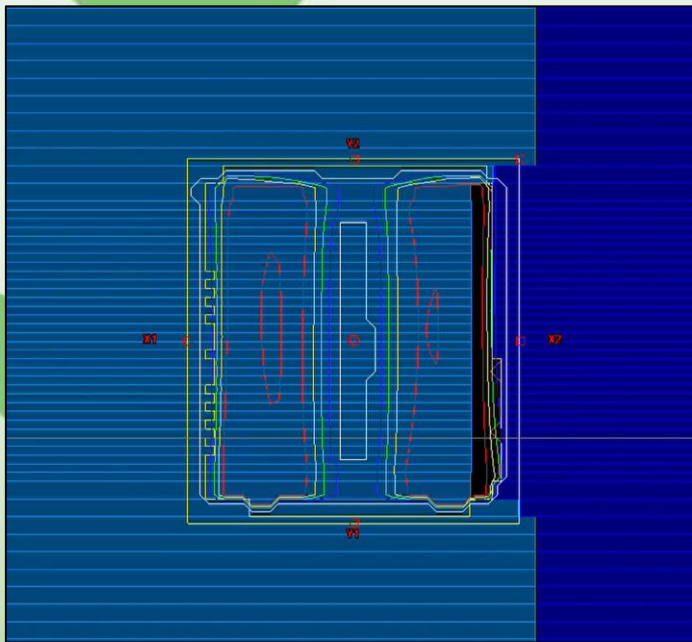
Modulated beams



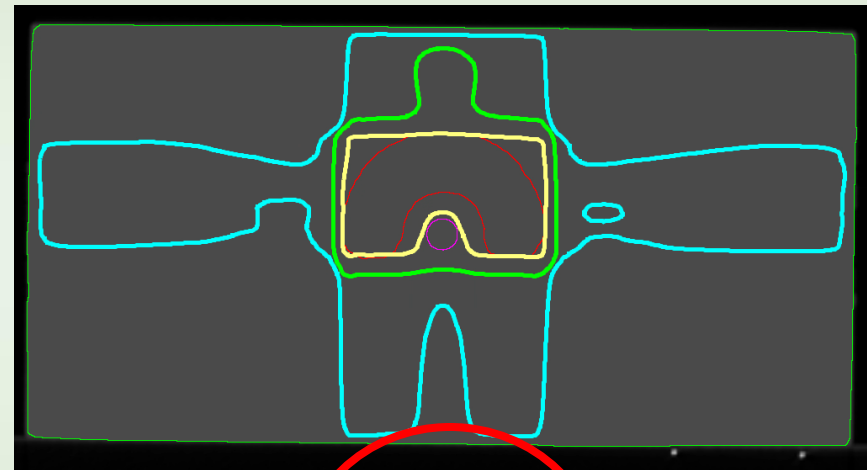
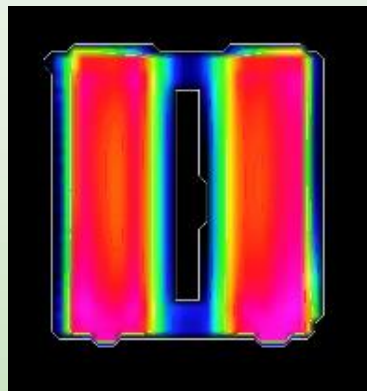
Superior sparing of normal tissue

Beam modulation

Intensity modulation can be achieved with dynamic MLC motion



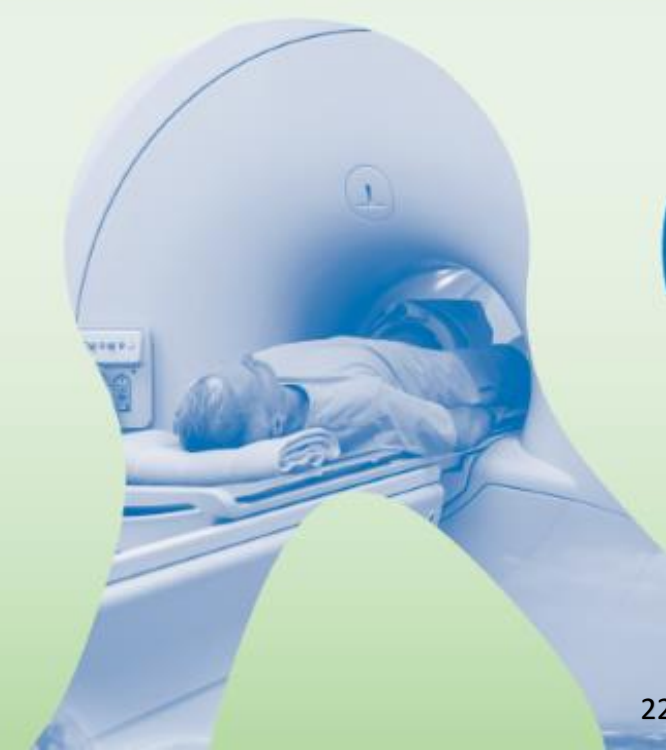
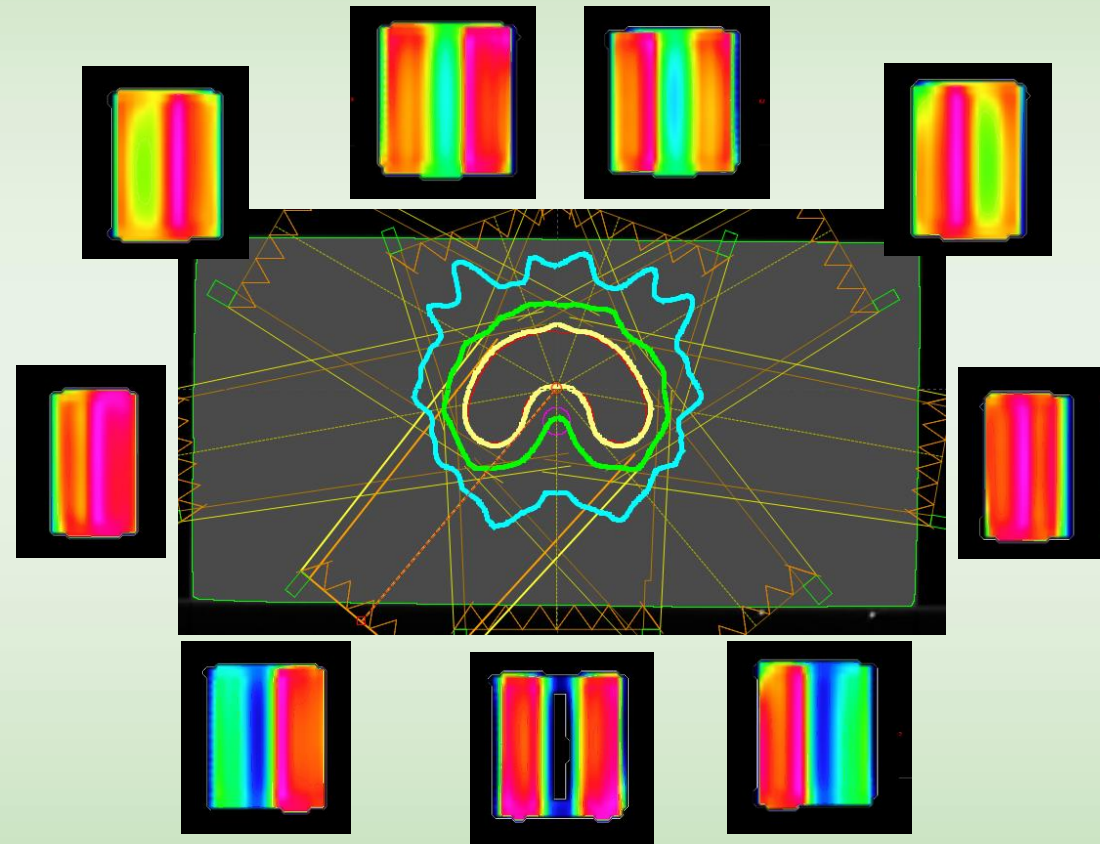
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Intensity modulated RT (IMRT)



- Multiple modulated beams = optimal sparing of normal tissue

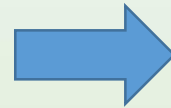
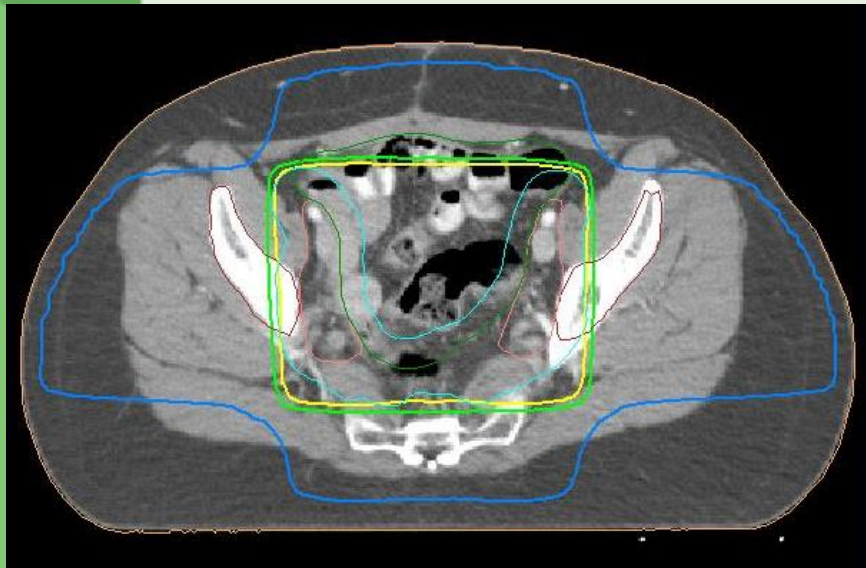


Intensity modulated RT (IMRT)

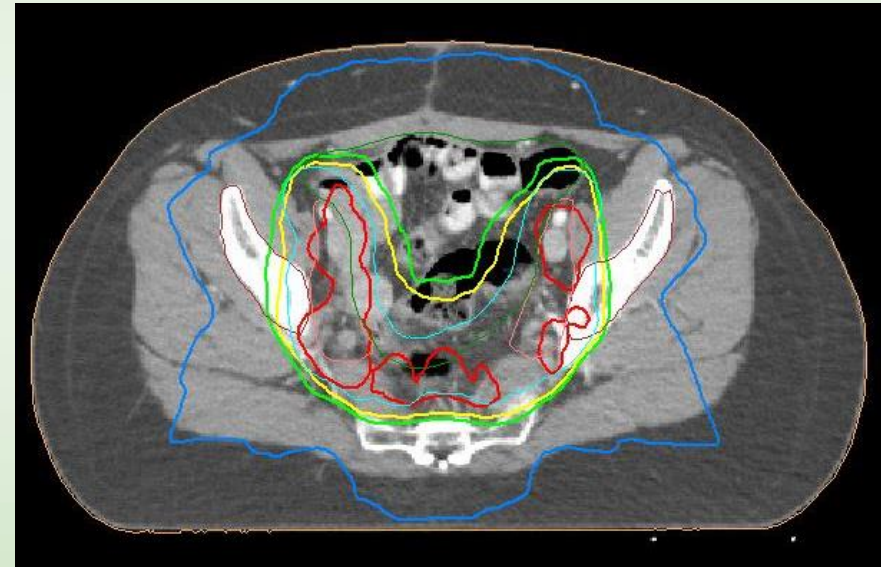


- IMRT: 1990s-2000s (first in Brazil in 2000)
- Better conformality to target and sparing of normal tissue

Conformal (3D)



IMRT



- Done in about 55% of services in Brazil

Modulated arc therapy (VMAT)



- VMAT 2000s-2010s (first in Brazil in 2010)
- Dynamic gantry rotation + MLC motion + dose rate variation
- Combines high modulation with delivery speed

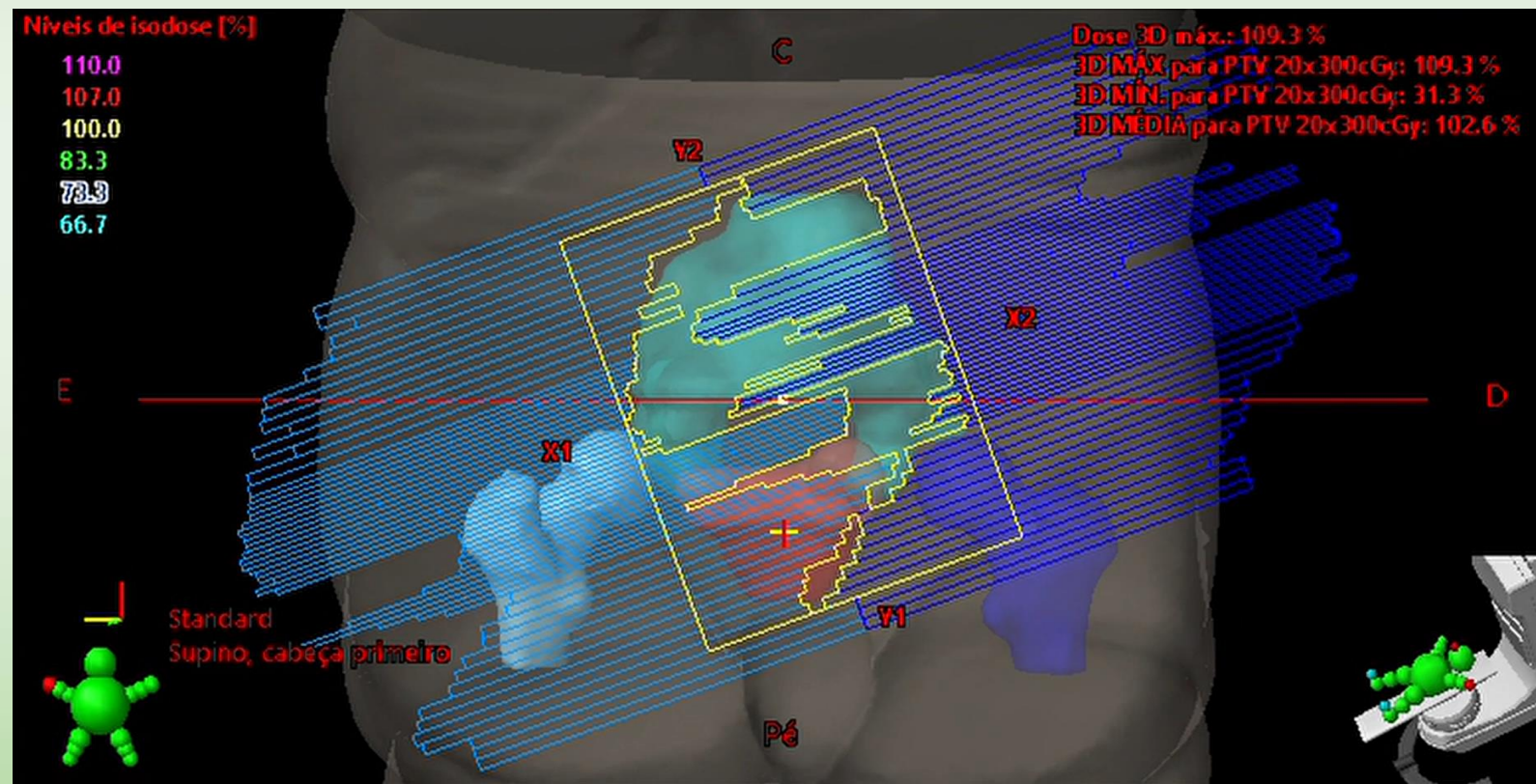
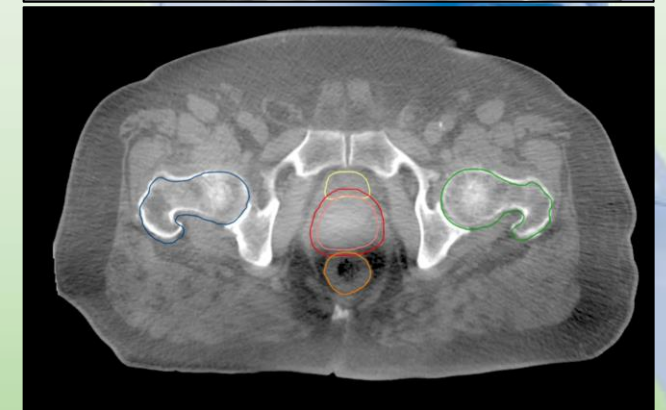
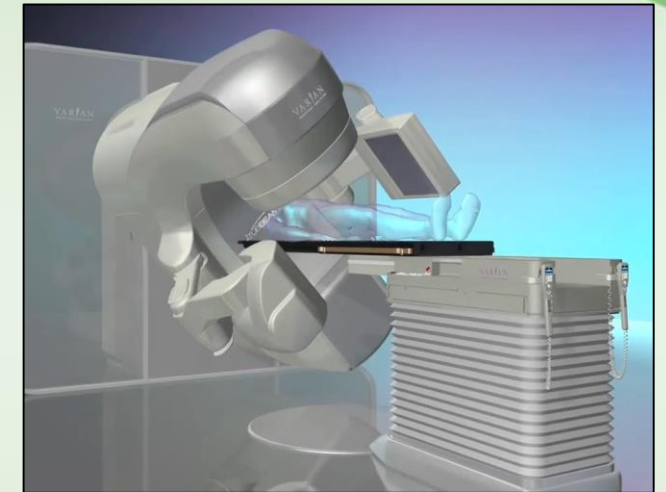
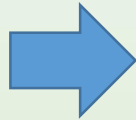
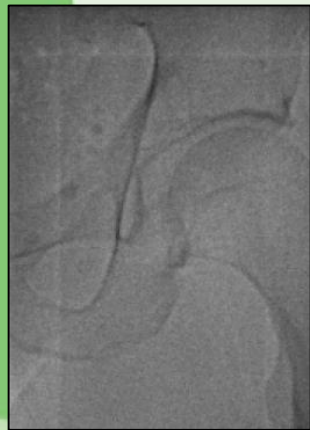


Image-guided RT (IGRT)

- Quality image guidance allows smaller margins
- MV image → On-board kV image → Cone-beam CT

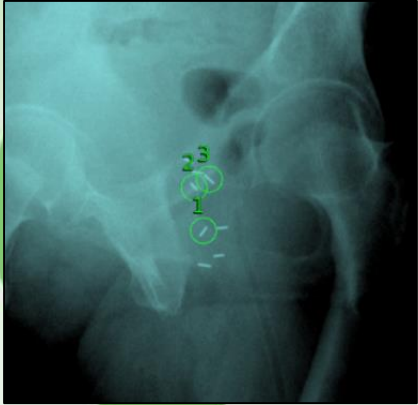
First in Brazil in 2007



IGRT

- Main contributing factor for the precision of modern RT
- Several modalities of image guidance available
- Many hardware developments in the last few decades

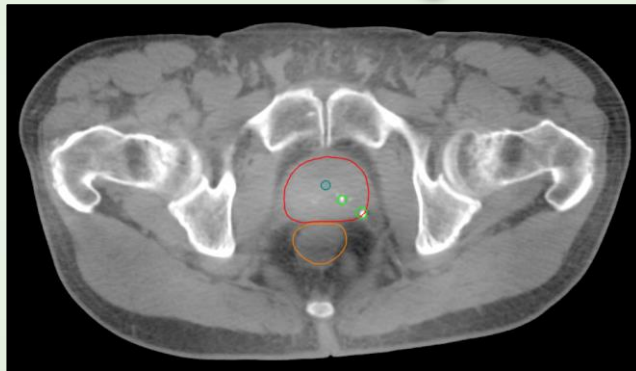
Fiducial matching/tracking



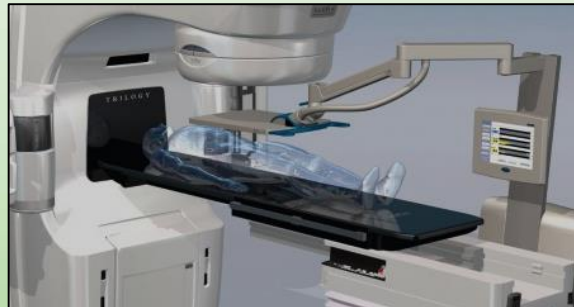
Surface guidance



CBCT 



Transponders



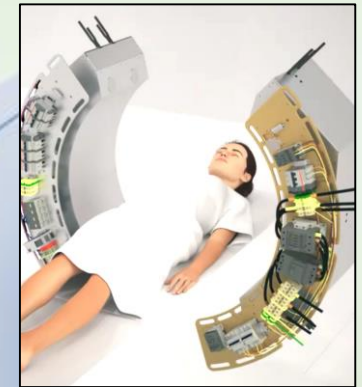
MRI-Linacs



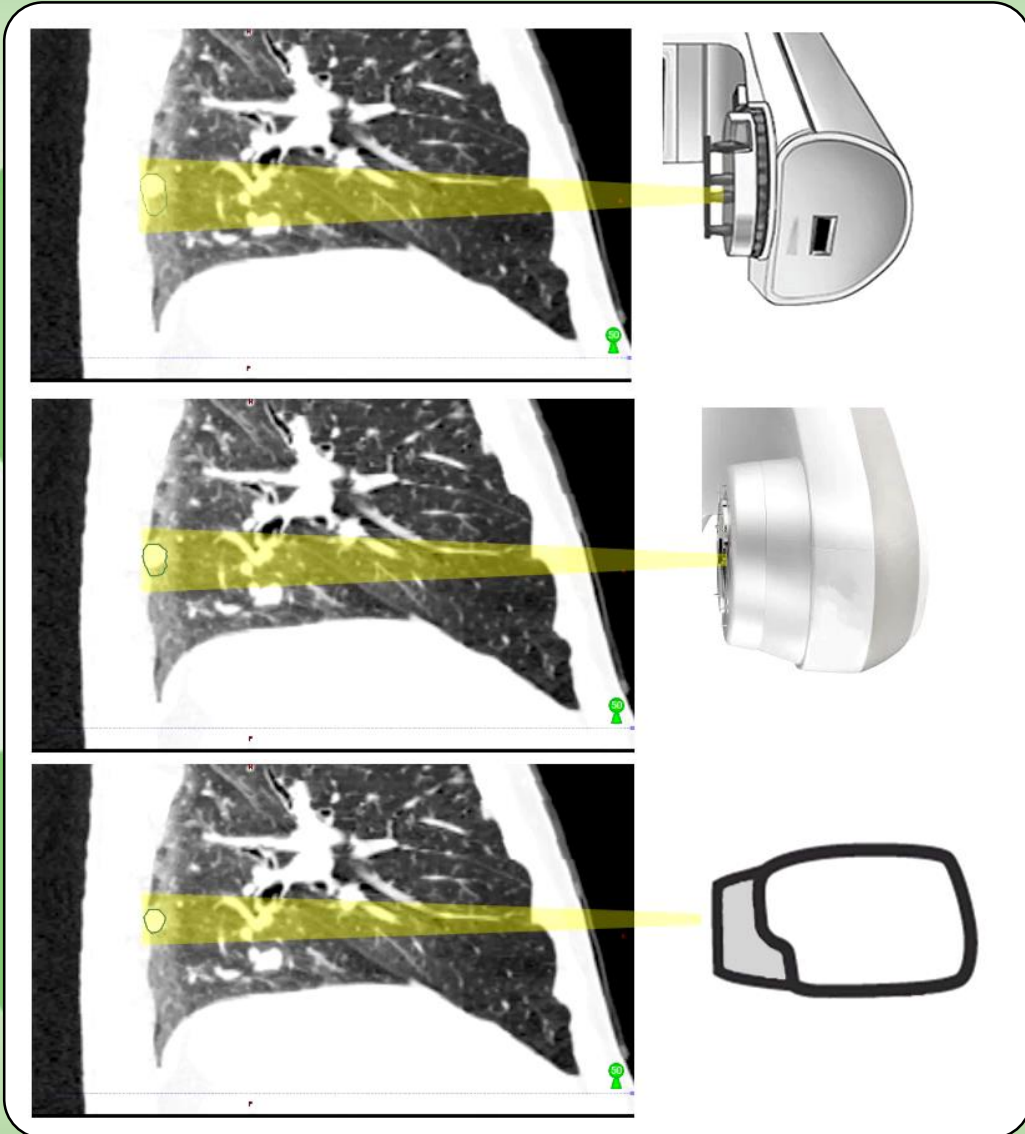
Ultrasound



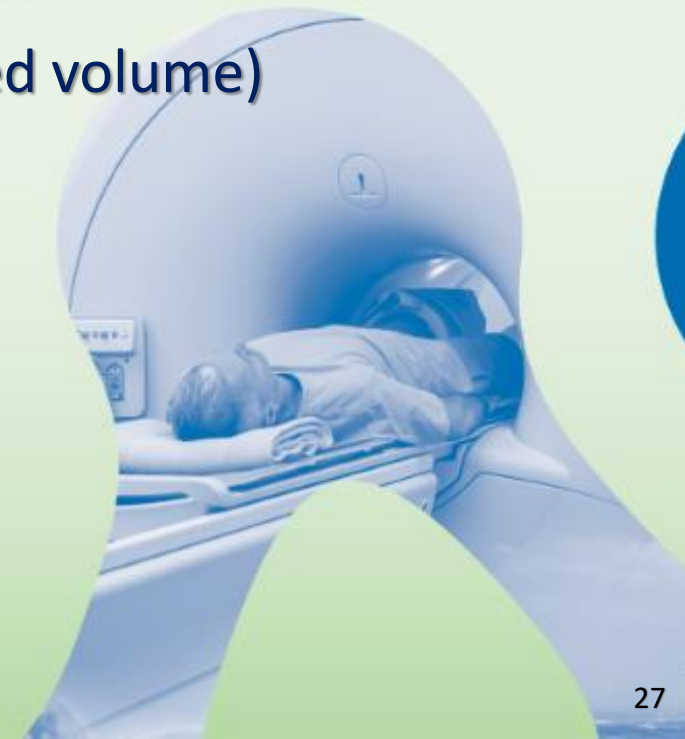
PET-Linacs



Breathing motion



- Moving targets pose a challenge in sparing normal tissue
- Motion management (reduction of irradiated volume)
 - Gating
 - Tracking



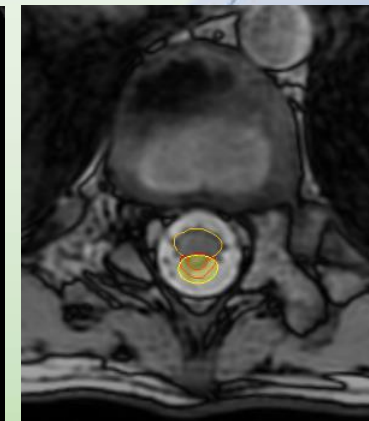
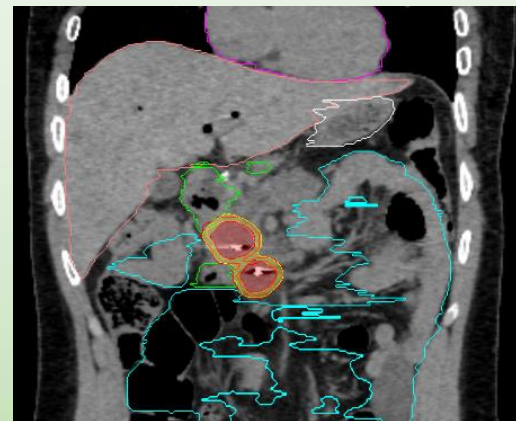
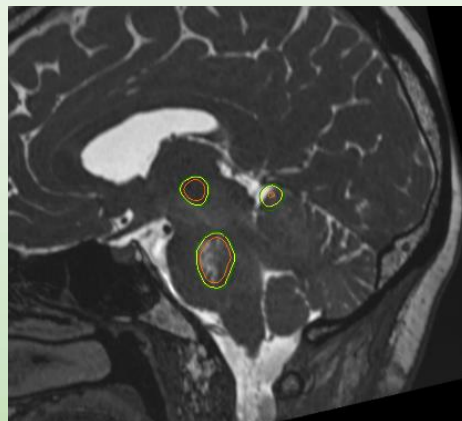
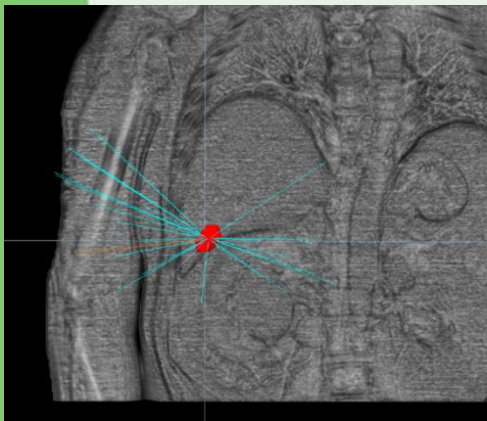
Hypofractionation

- Technology advances have enabled more precise treatments
 - Intensity modulation
 - Image guidance
 - Tighter mechanical accuracy
- Safe use of **higher doses in fewer fractions** (hypofractionation and radiosurgery)

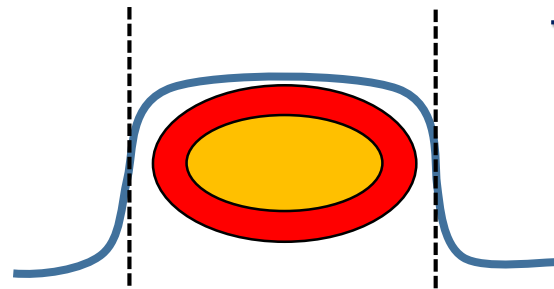
The application of different hypofractionation schemes is a major trend in clinical practice

Ex: Prostate

40 fractions → 20 → 5 → 1

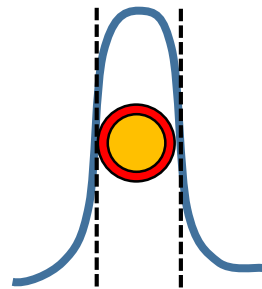


Radiosurgery and ablative RT



Conventional RT

- Large margins
- Homogeneous dose with smooth dose falloff

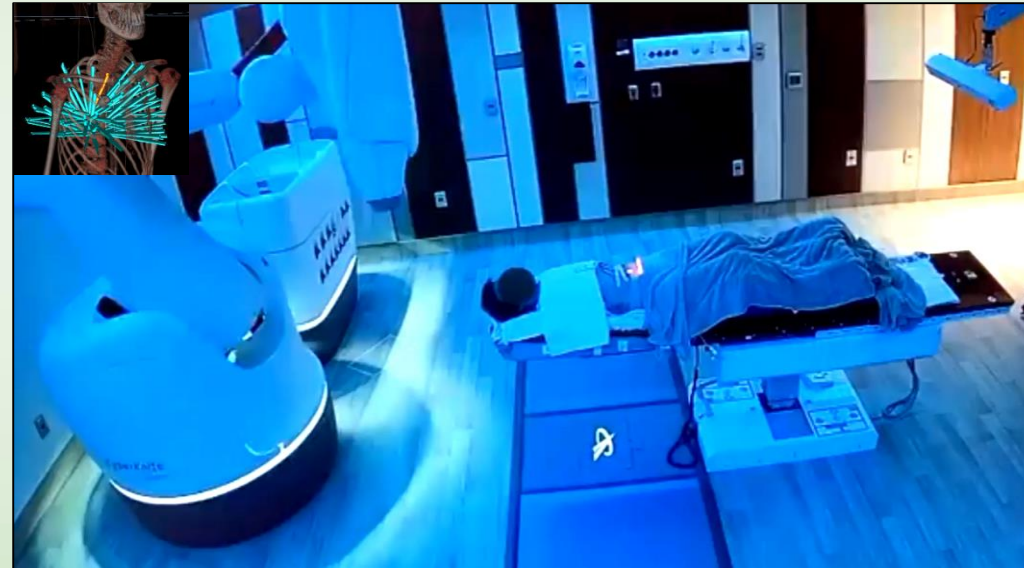


Stereotactic ablative RT (SABR)

- Tight margins
- Heterogeneous dose with sharp dose falloff
- Much less dose outside the target
- **Geometric miss is more severe**

Special LINACs: CyberKnife

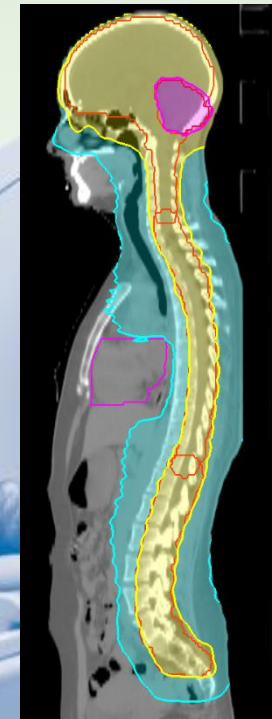
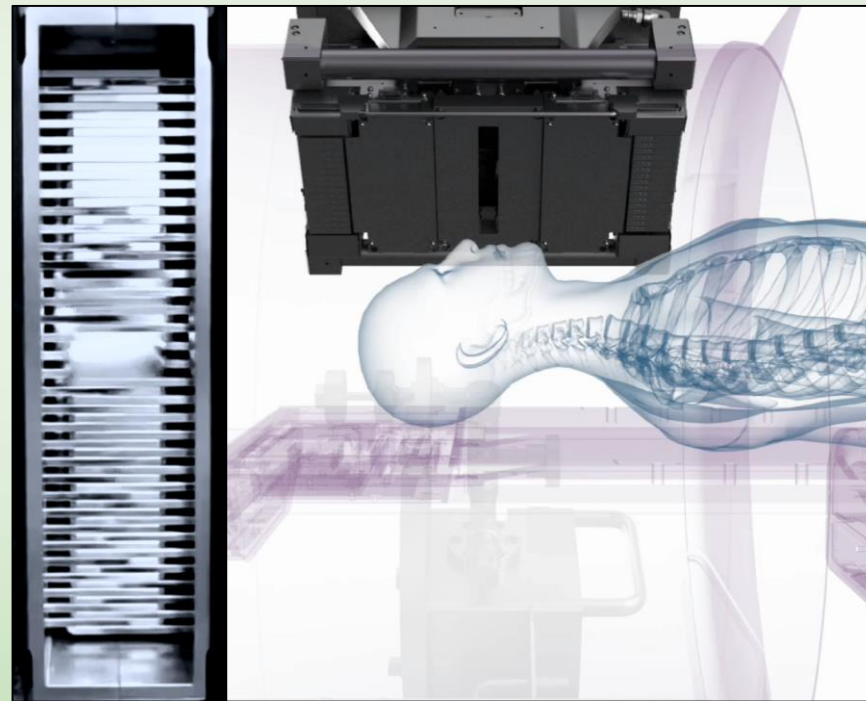
- Robotic tracking
- Automatic detection and correction of offsets in near real time
- Continuous compensation of breathing motion



- Only 1 in Brazil

Special LINACs: Tomotherapy

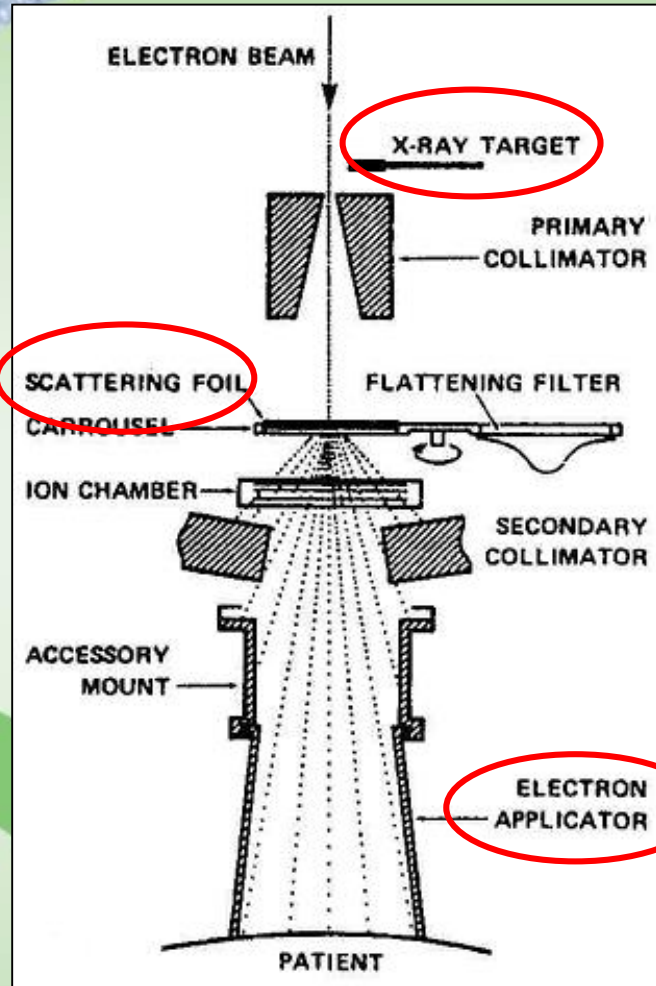
- Helical delivery of fan beam with fast binary MLC
- Superior capability of beam modulation
- Continuous compensation of breathing motion



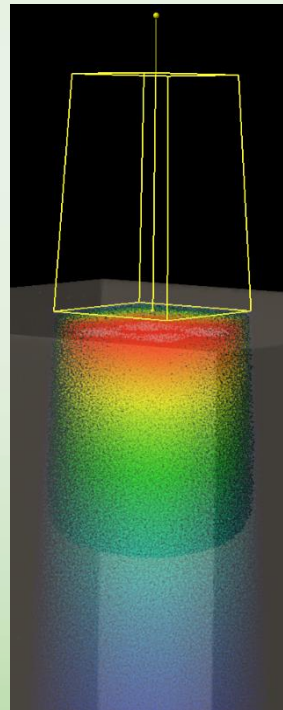
- Only 1 in Brazil

Electron Beams

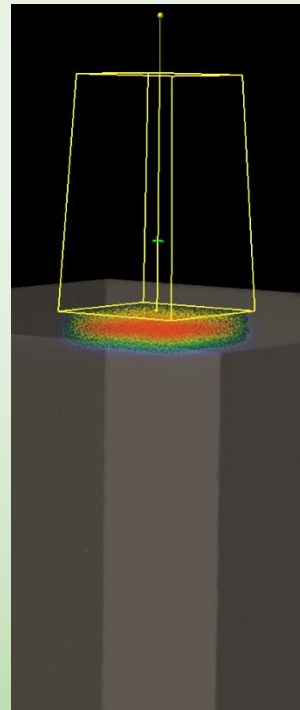
- Shallow dose distribution, rapid dose falloff
- Easy to shield with a few mm of lead
- Used for skin and superficial targets



X-Rays



Electrons



Intraoperative RT (IORT)

- Conventional Linacs (electron beam)
- Brachytherapy
- Dedicated mobile units

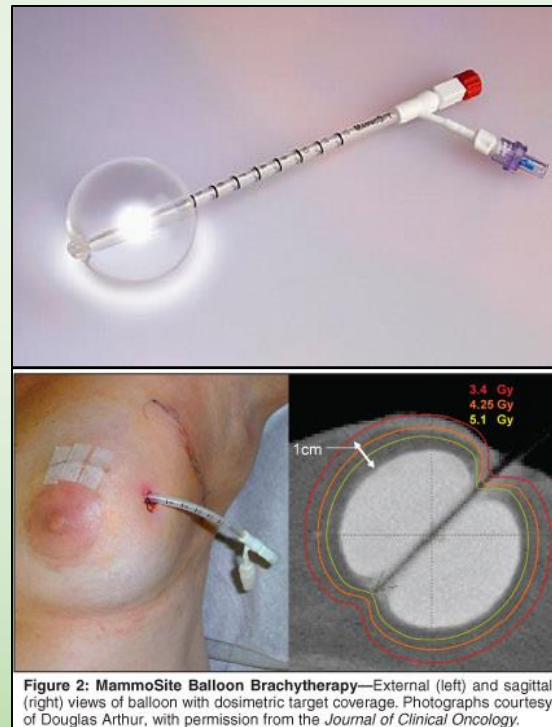


Figure 2: MammoSite Balloon Brachytherapy—External (left) and sagittal (right) views of balloon with dosimetric target coverage. Photographs courtesy of Douglas Arthur, with permission from the *Journal of Clinical Oncology*.



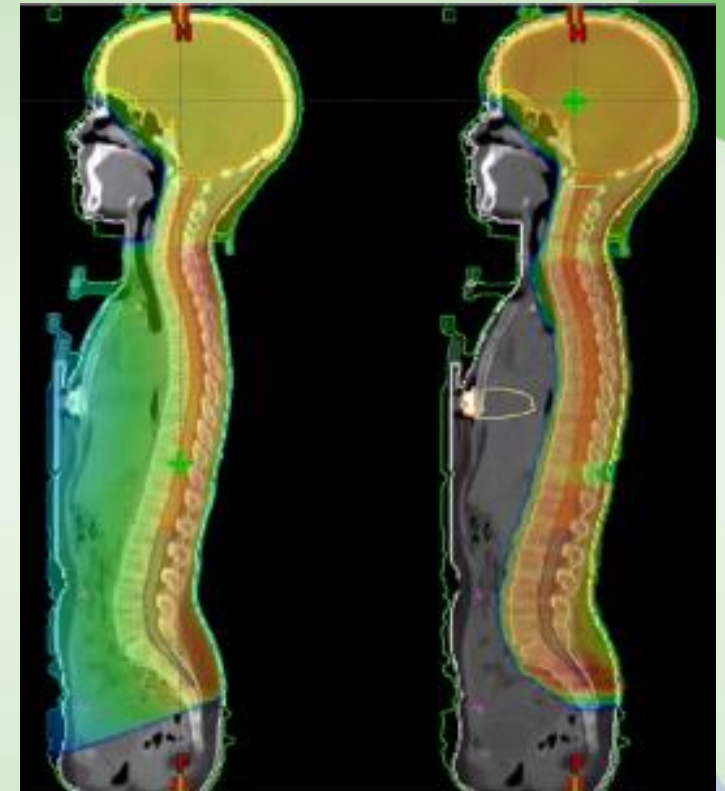
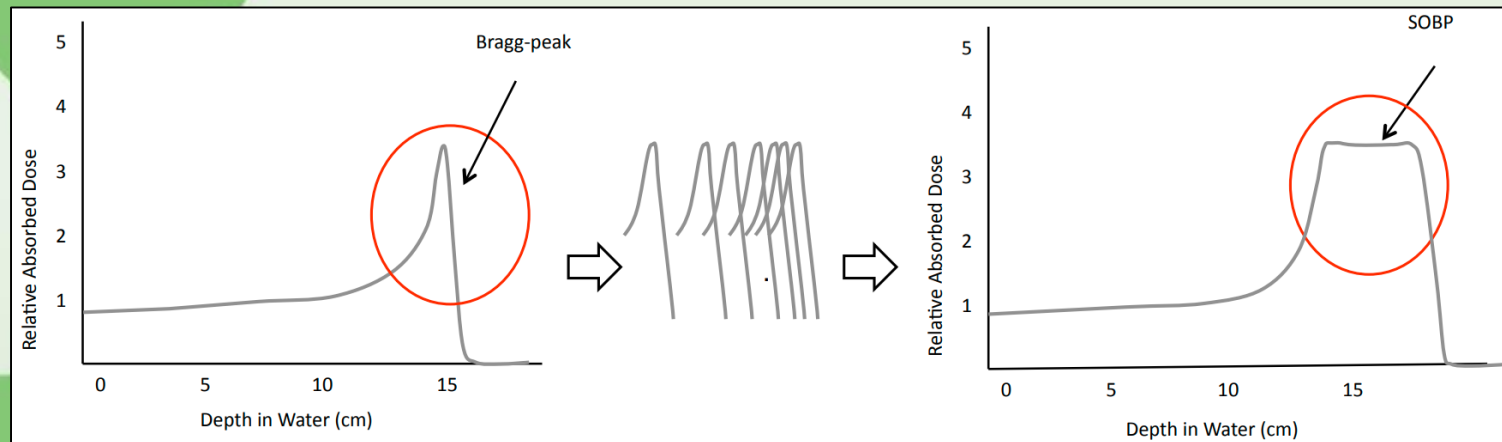
Proton therapy



- Protons and heavy ions → Bragg peak
- Deep range with virtually zero exit dose
- Range depends on energy

X-Rays

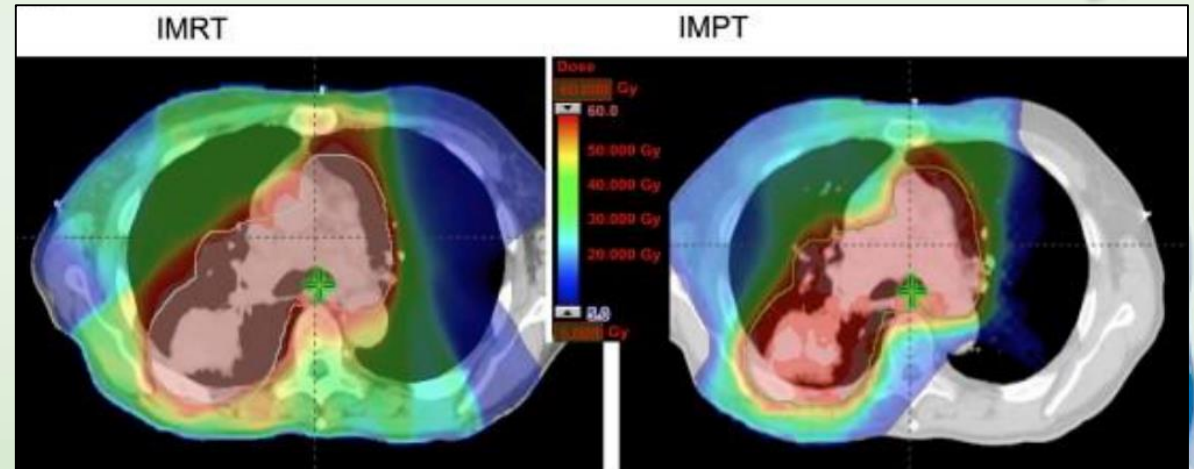
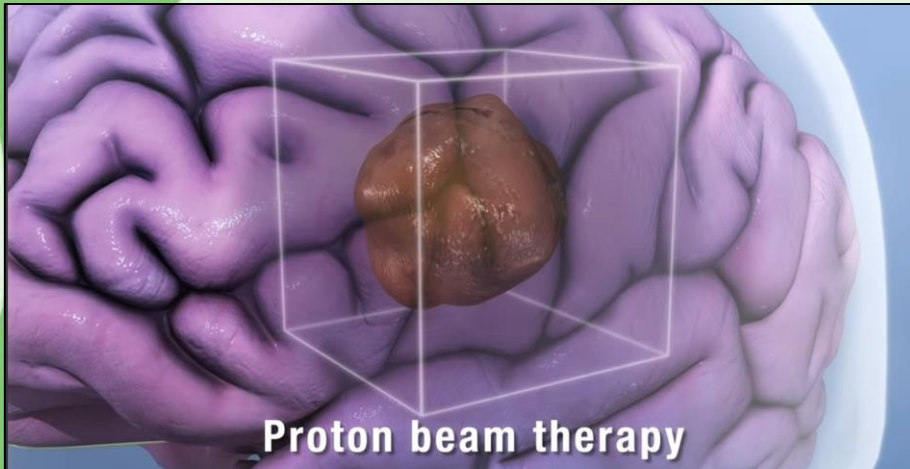
Protons



Kumar JPHO 2013

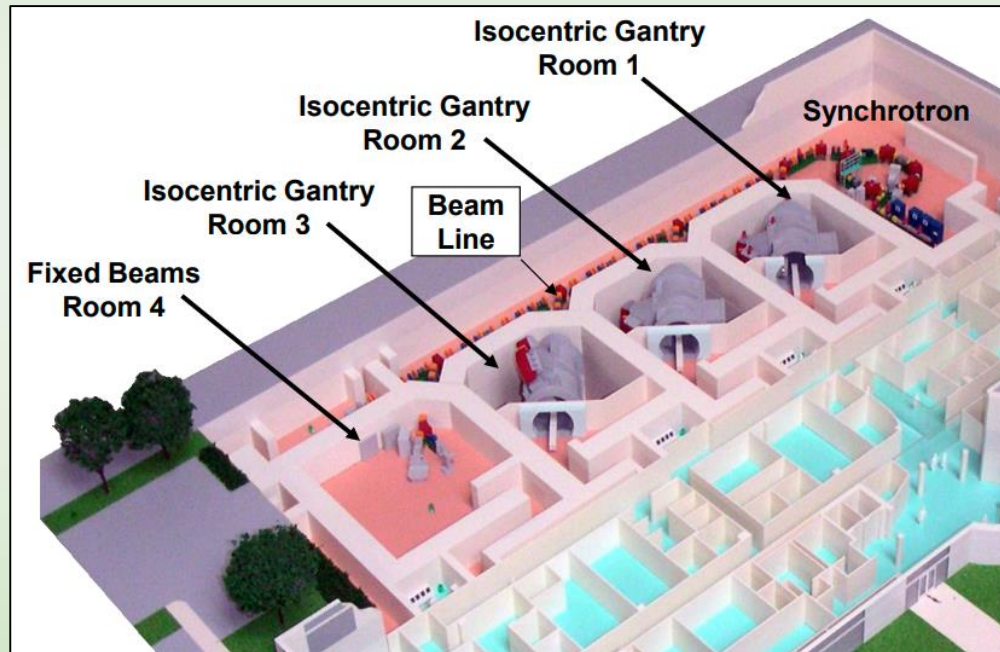
Proton therapy

- Pencil beam scanning: dose conformity possible with even a single beam
- Intensity modulated PT: potential to minimize integral dose
- Challenge: uncertainties (particle range, biological effectiveness, plan robustness, motion management)



Proton therapy

- Biggest challenges: cost and size
- Most current facilities are dedicated regional PT centers with multiple treatment rooms



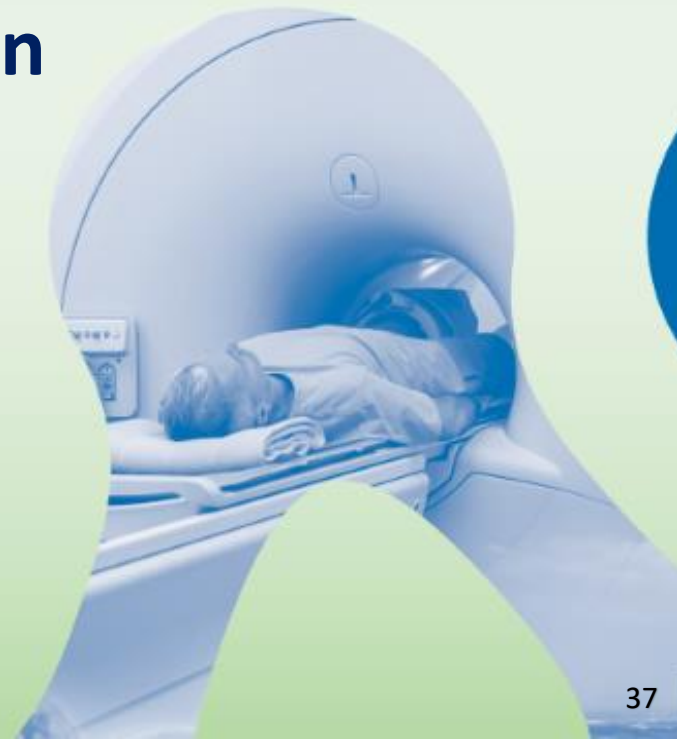
MD Anderson Proton Center

- None in Brazil (nor Latin America)



Future directions

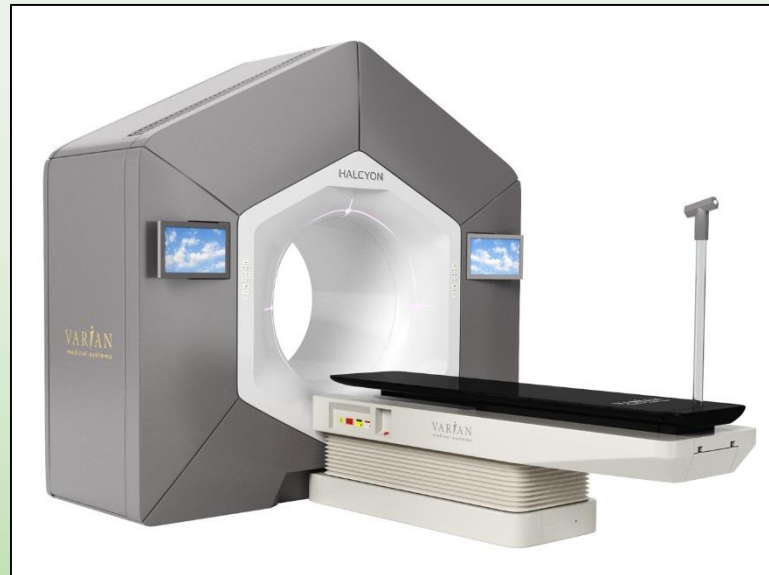
- Most research efforts are in the use of artificial intelligence software (won't be covered here)
- Currents trends in treatment delivery hardware:
 - Improved workflow and cost reduction
 - Better imaging and adaptive RT
 - Ultra-high dose rate (FLASH)



Linacs: Simpler can be better



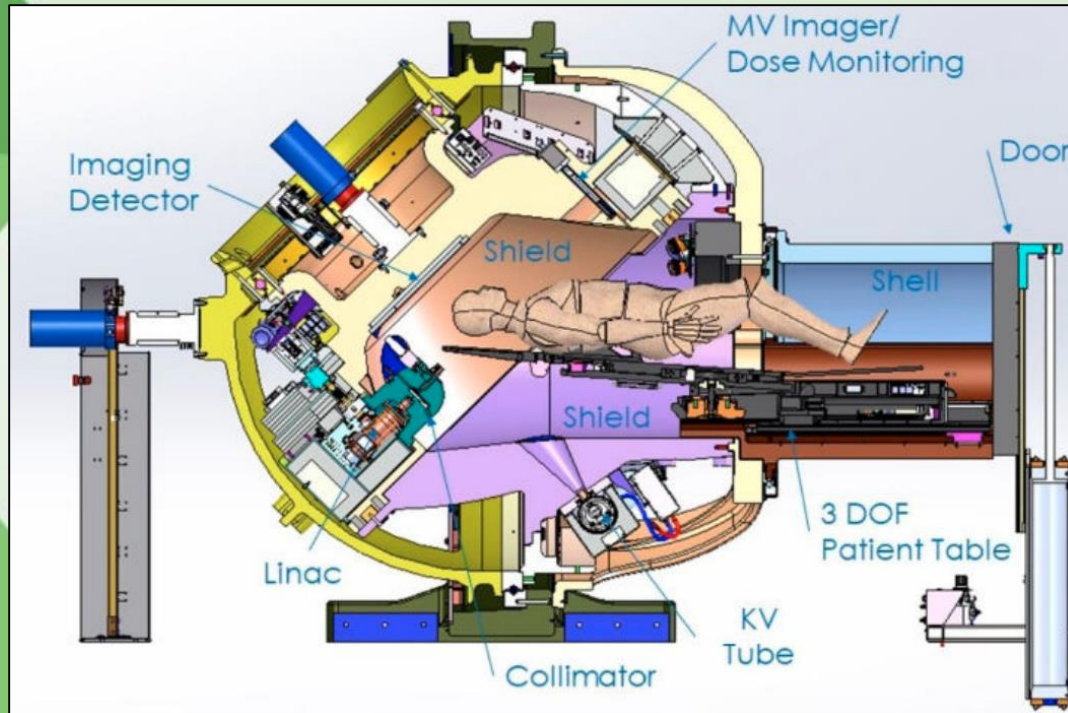
- Compact blueprint (single energy, no couch rotation, self-shielded)
- FASTER! (fast rotation, faster imaging, fast modulation)
- Maintenance: modular parts (replace instead of repair, increase uptime)
- Reduced or simplified features, but still advanced machines
- Reduce costs and treatment time to make technology more available



ZapX



- Compact vaultless gyroscopic radiosurgery Linac



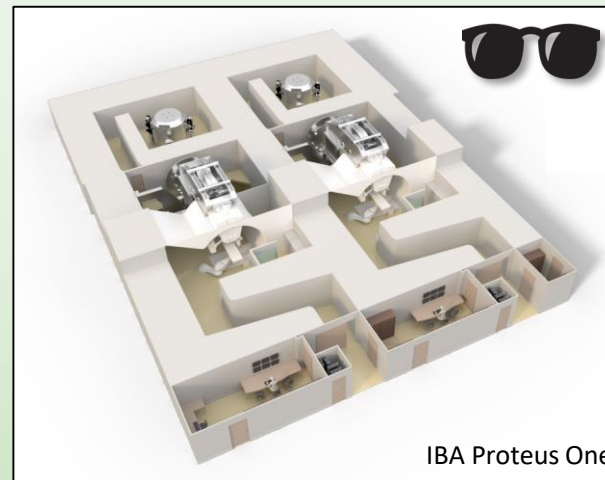
Protons: Smaller and cheaper

- Price of acquiring proton therapy treatment has greatly decreased, but is still unaffordable in most settings (in the order of 10^7 to 10^8 USD)
- Room size requirements have decreased dramatically

Specialized proton centers



Dedicated proton rooms



IBA Proteus One

Replacing old Linacs in existing rooms

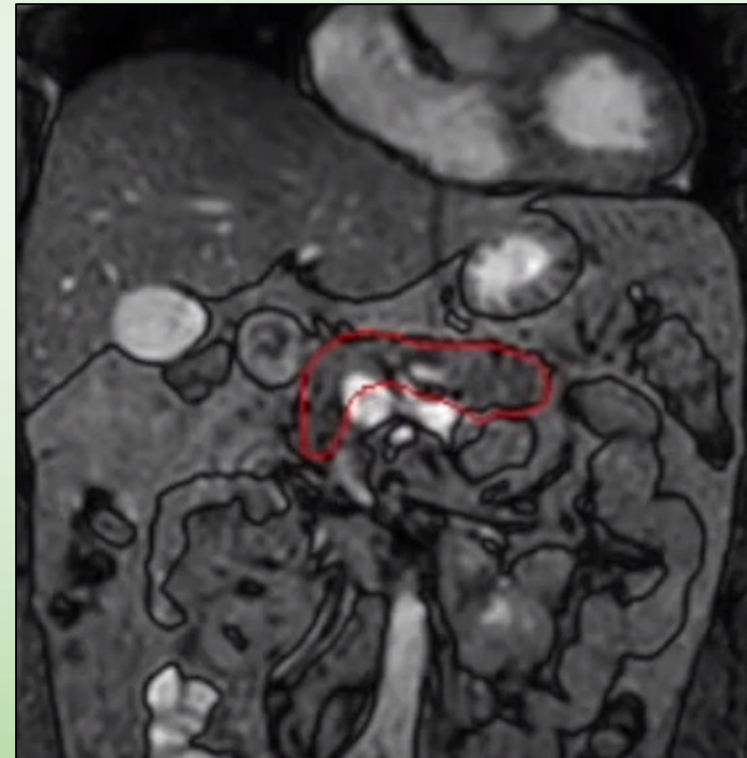
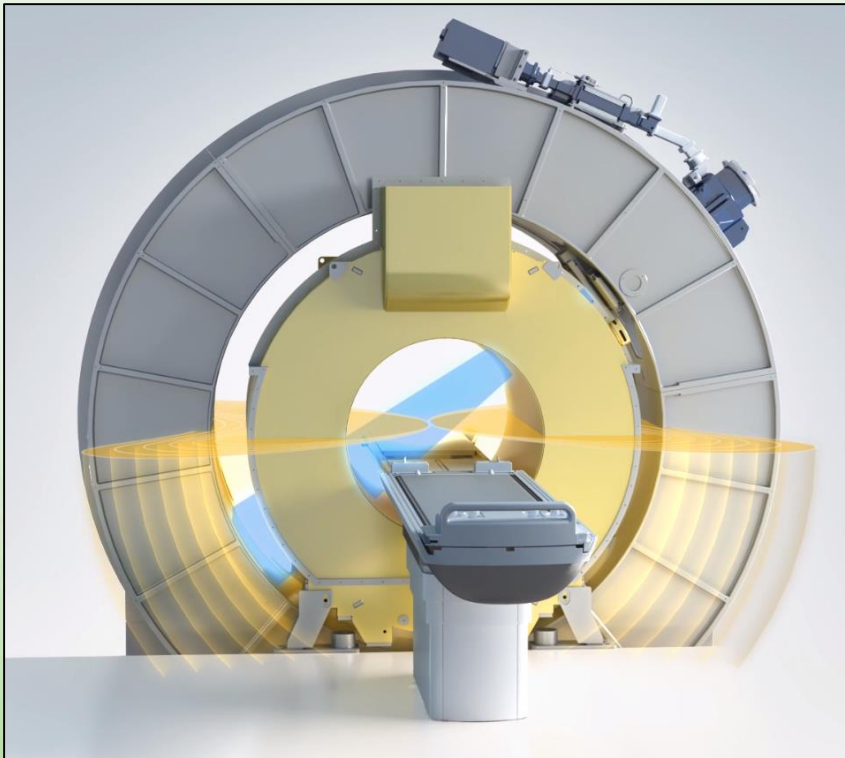


P-Cure

Magnetic Resonance guided RT



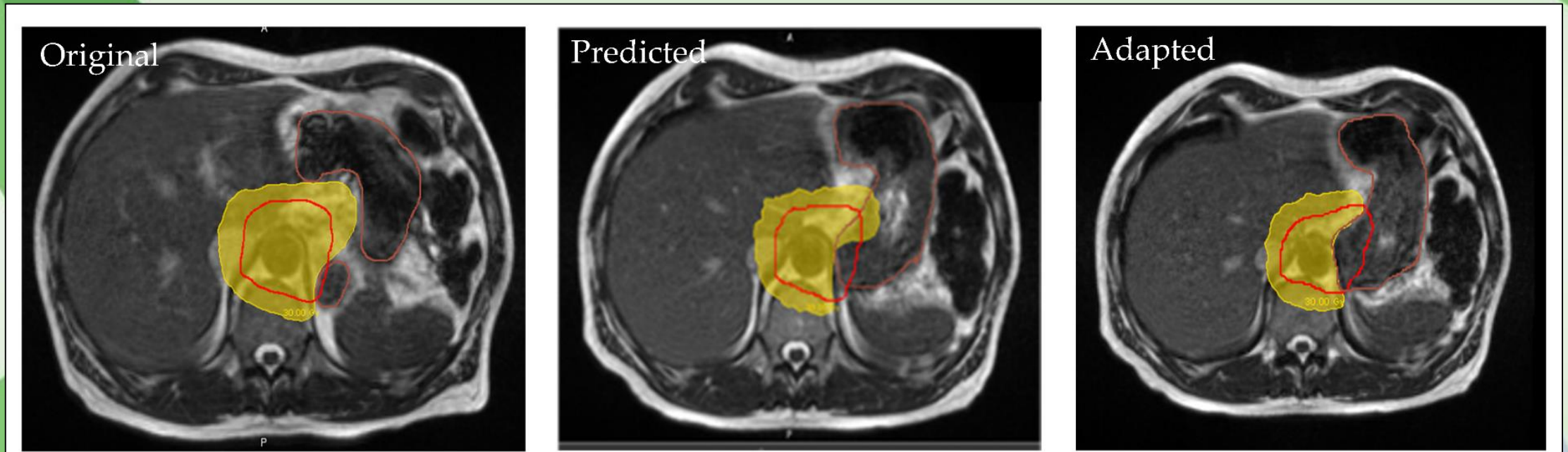
- LINAC + MRI
- Better target definition and real-time motion assessment
- In development for a couple of decades due to MANY engineering challenges, but finally becoming mainstream



MRgRT

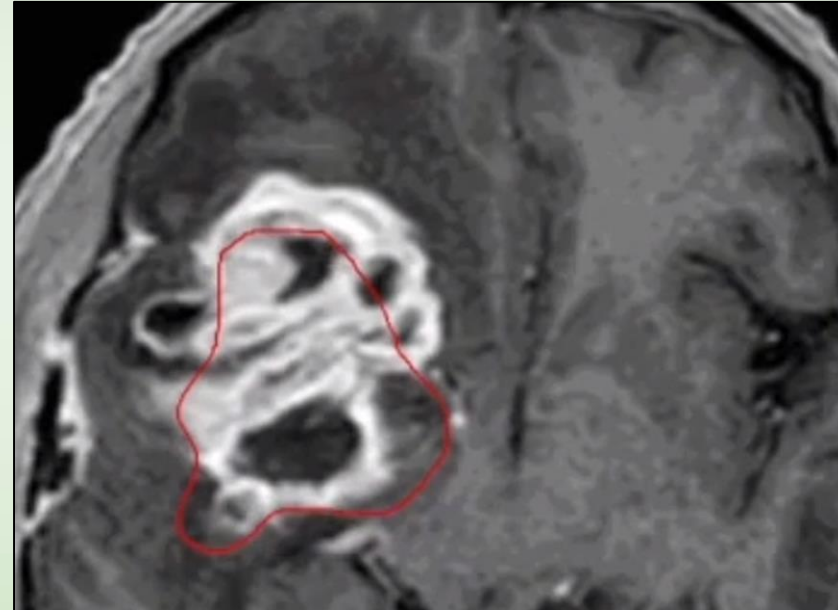
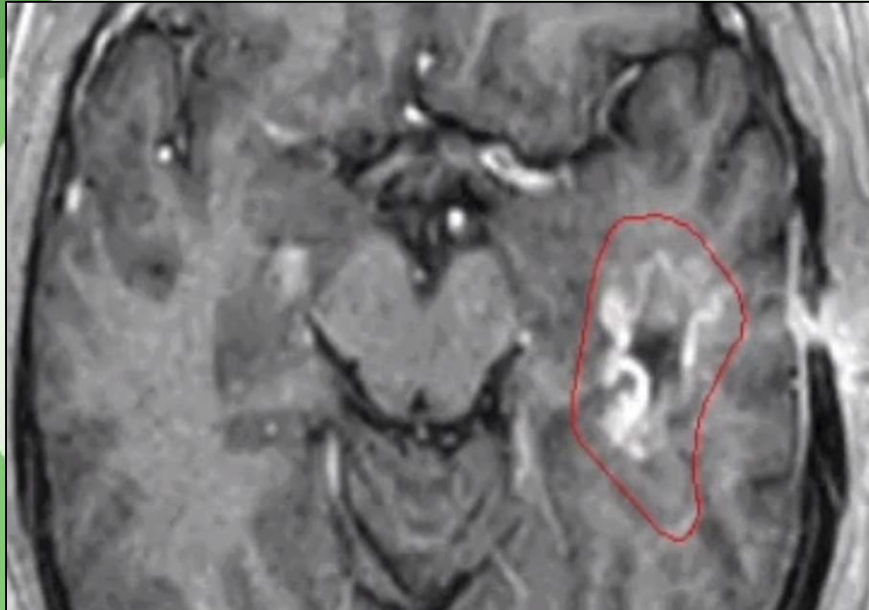


- Daily online plan adaptation to target position and deformation



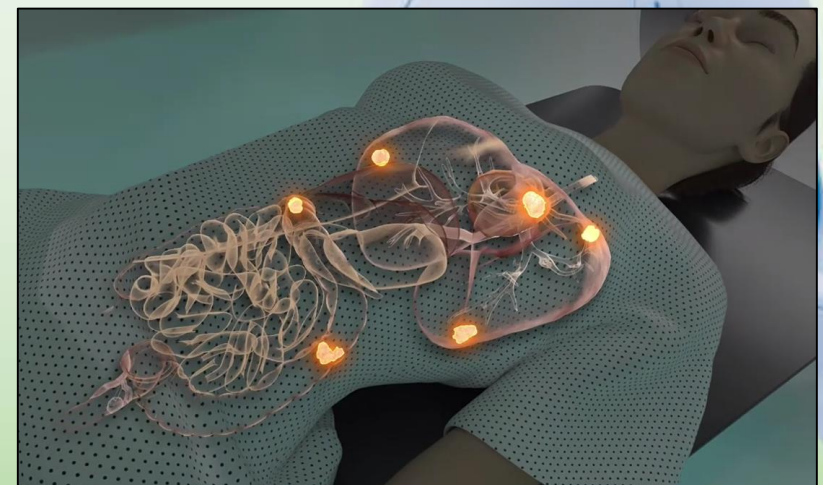
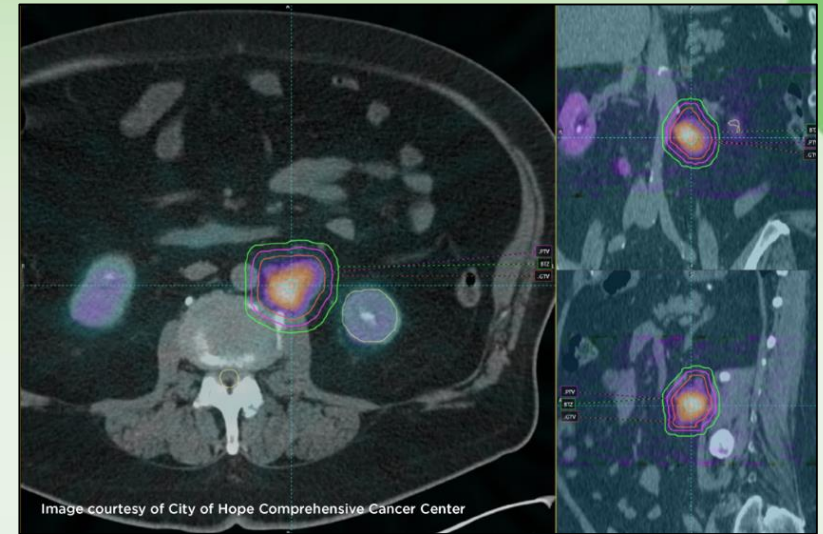
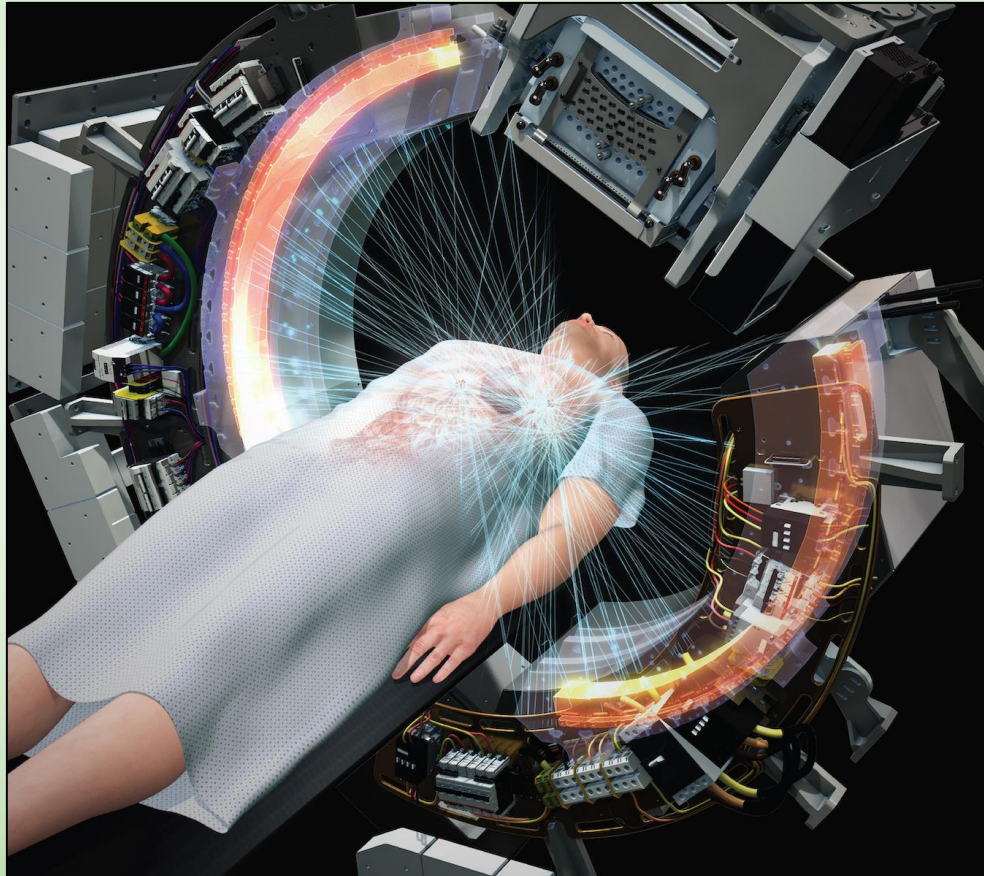
MRgRT

- Online assessment and adaptation of target response
 - Shrinkage/growth 🕶️
 - Biomarkers 🚀



Biological guided RT (BgRT)

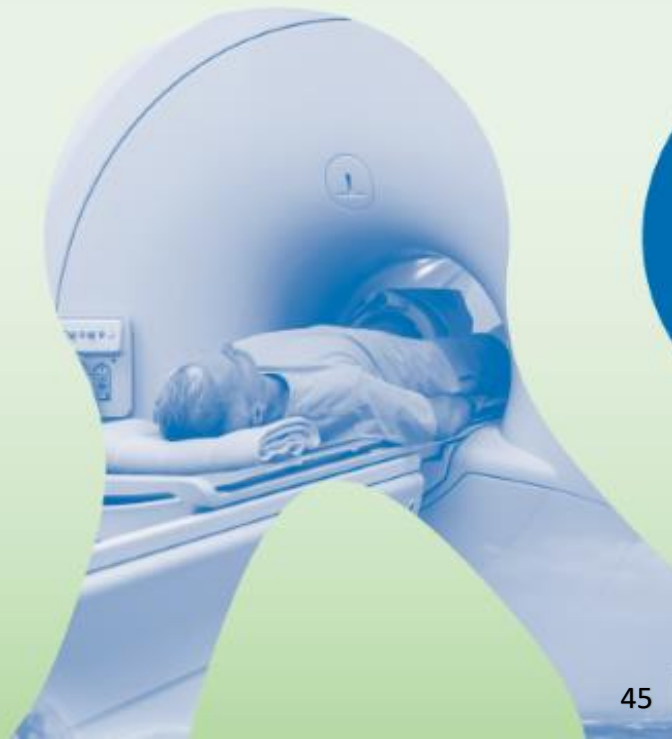
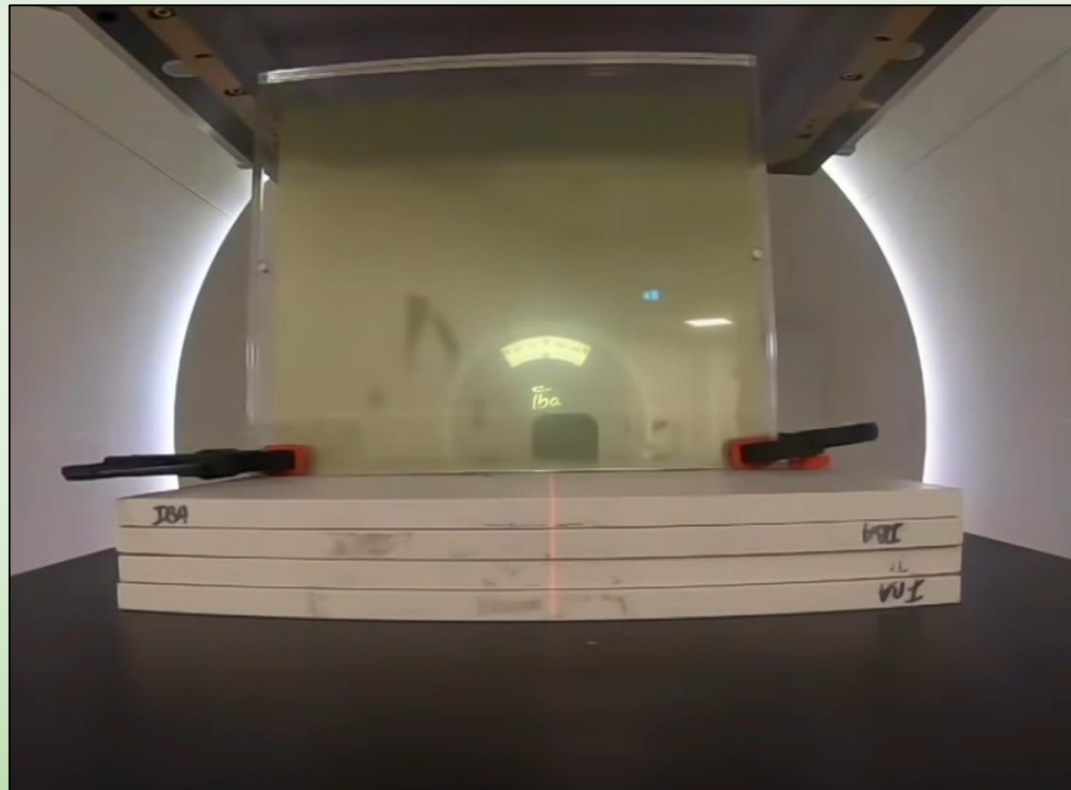
- LINAC+PET
- Identify, adapt and track “active” regions



Ultra High Dose Rate (FLASH)



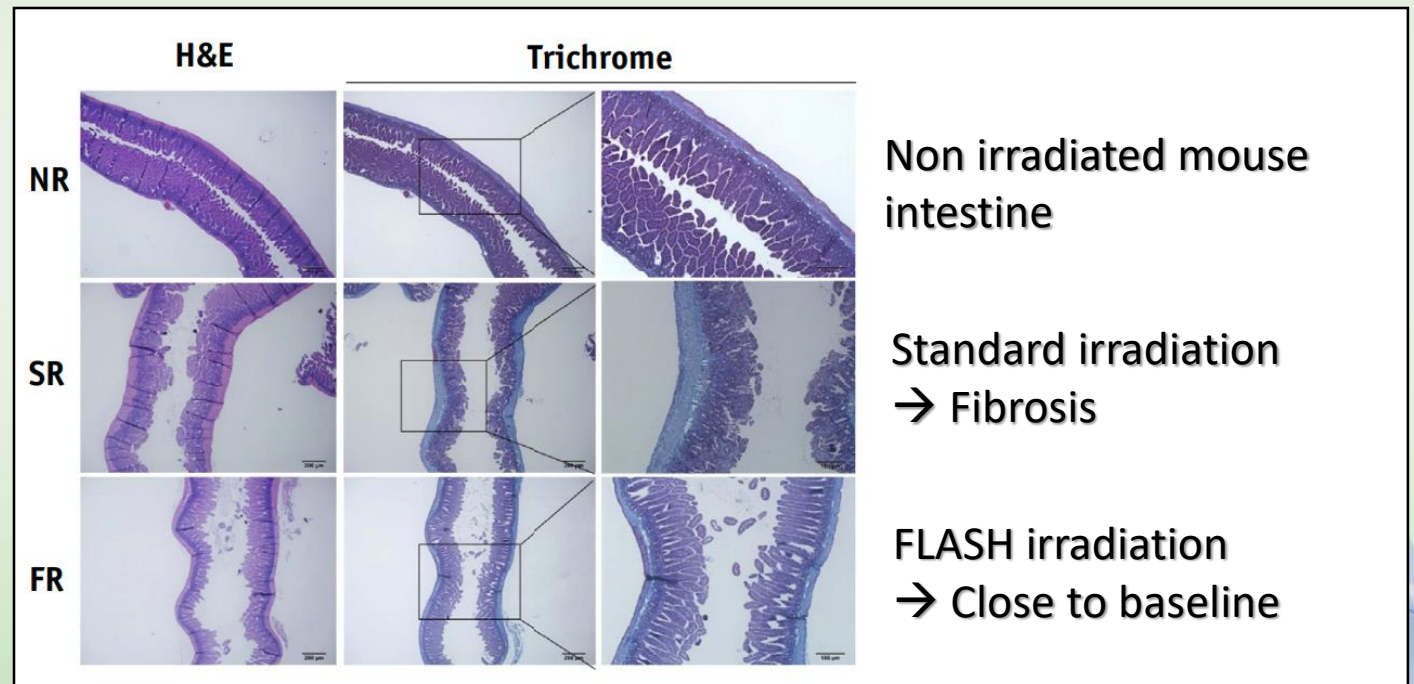
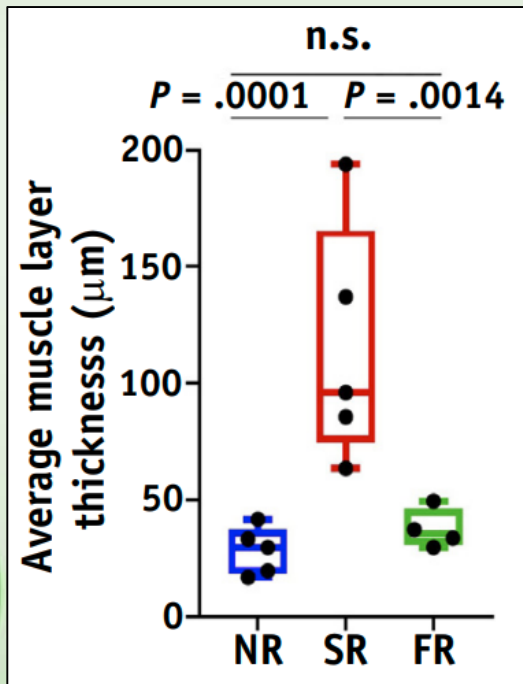
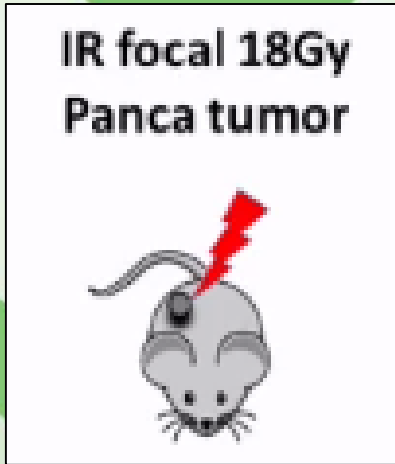
- Typical dose rate of SRS Linac $\approx 10\text{Gy}/\text{min}$
- FLASH: $40\text{-}100\text{Gy}/\text{s}$ (“clinical”) (can reach $>10^3\text{Gy}/\text{s}$)
- Treatment delivery in a few ms \rightarrow further improve precision therapy?



FLASH effect



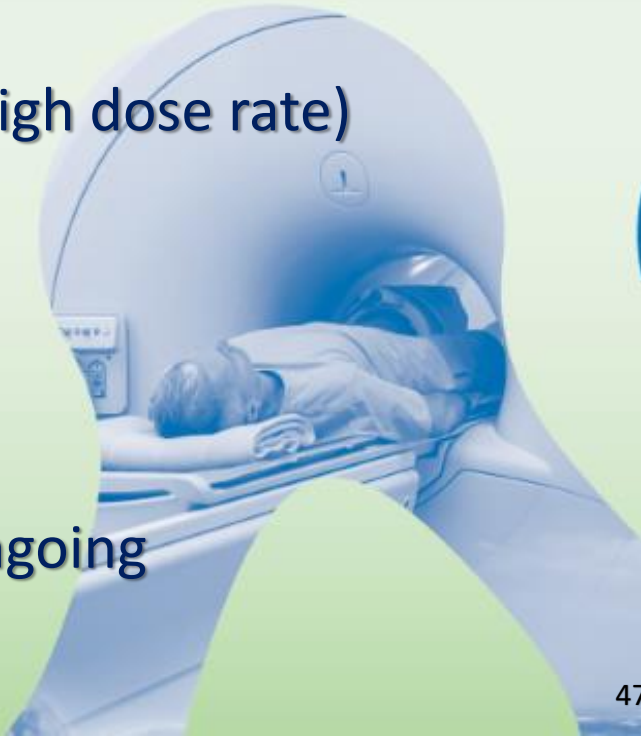
- Evidence of better normal tissue sparing, not yet fully understood
- Potential for sparing normal tissue within the field (i.e. using biology instead of avoiding the tissue and potentially underdosing the tumor)





FLASH Challenges



- Mostly done with **charged particles**
 - currently **unachievable with MV X-Rays** (bremsstrahlung yield and heat)
 - Electrons: limited to superficial lesions
 - Feasibility issues with pencil beam scanning and IMPT (effective dose rate to produce FLASH effect)
 - Quality assurance challenges (detectors for ultra high dose rate)
 - Currently: pre-clinical, transition
 - More questions than answers
 - Mostly animal studies
 - Feasibility studies and very limited clinical trials ongoing
- 

Thank you!



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